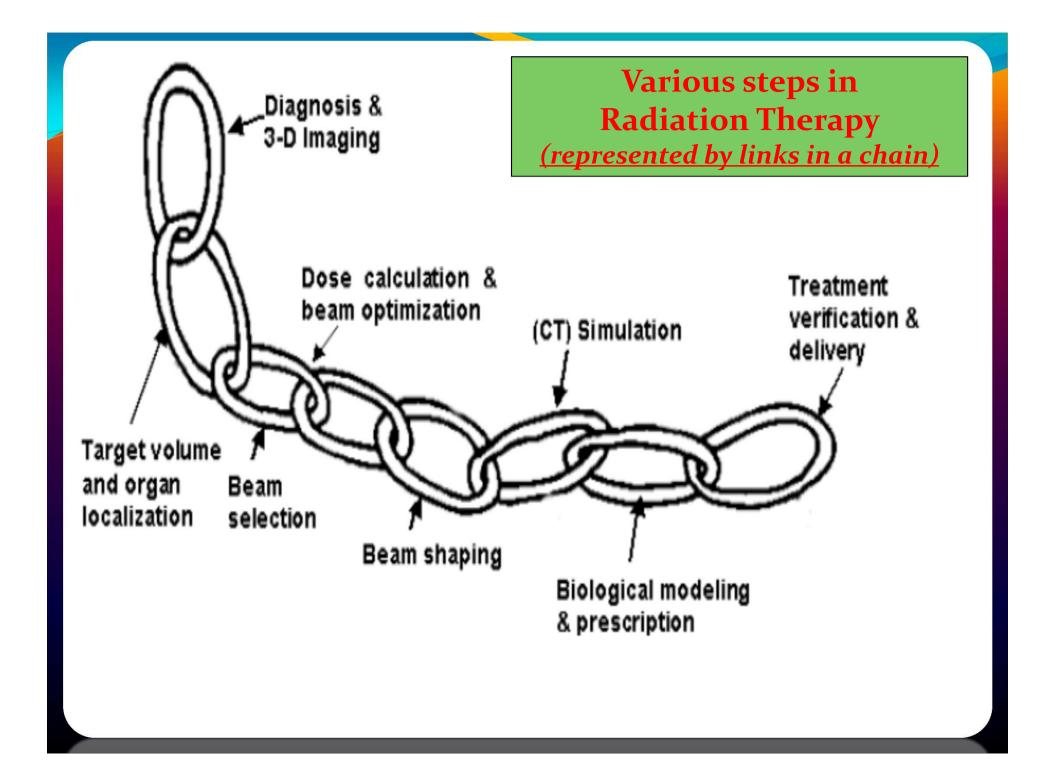
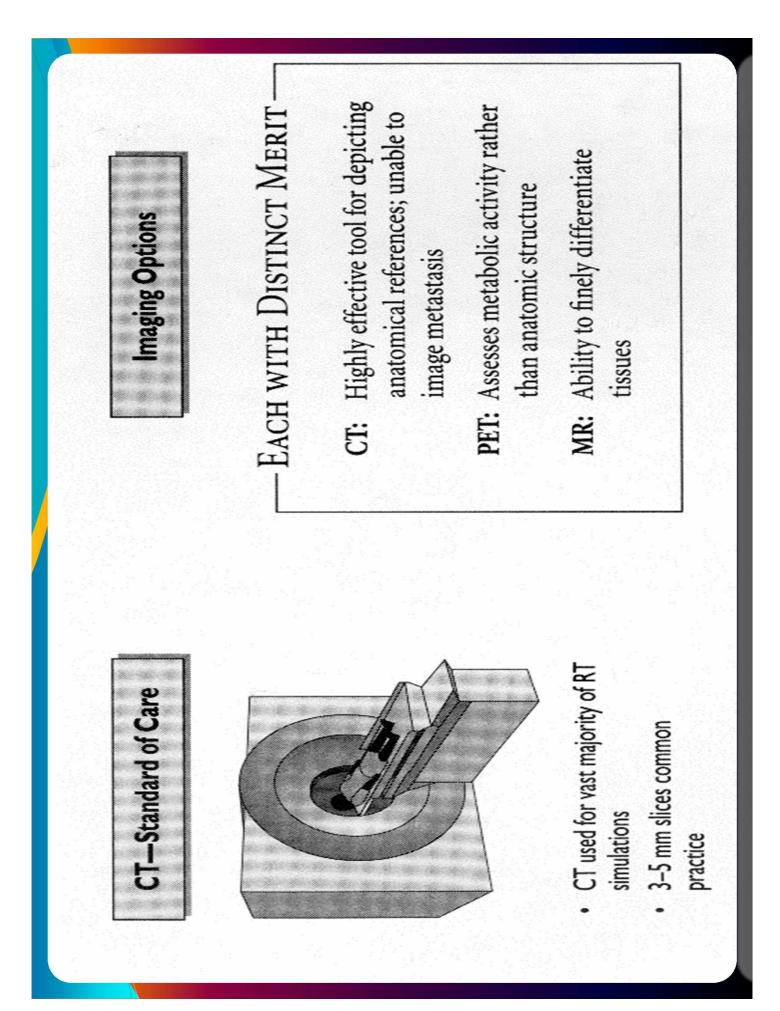
# Radiotherapy Treatment Planning -<u>An overview</u>

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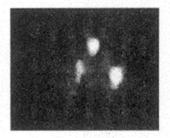






#### CT Scan

- Anatomical reference
- Tells physician exactly where lesion is located
- Improves specificity



#### **PET Scan**

- Metabolic reference
- Helps physician determine whether lesions are malignant or benign and identifies areas of cancerous involvement
- Improves sensitivity in detecting small lesions

#### Fusion: CT + PET

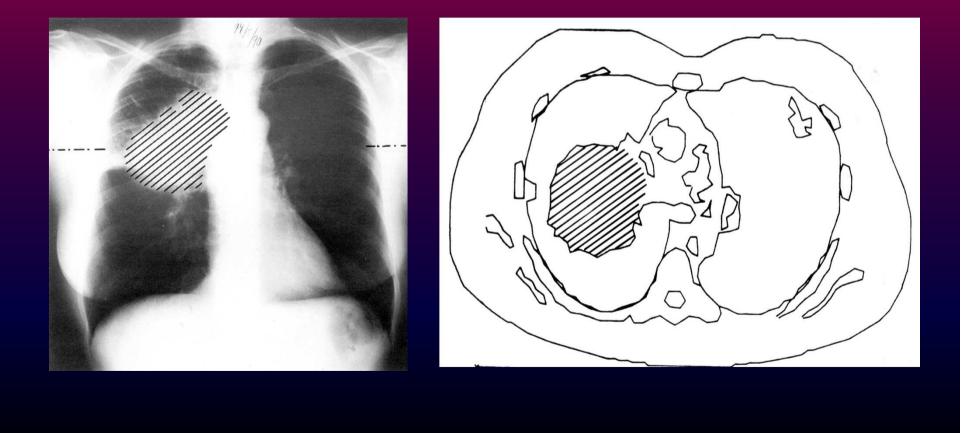


#### **Fused Image**

- Electronic fusion of CT and PET images
- Allows for direct visual comparison of two different data sets
- Image superposition/fusion allows for resizing and movement of data sets, as well as zooming and rotation to achieve optimal overlay of data

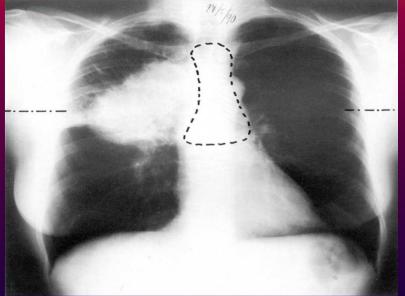
# **Gross Tumor Volume (GTV)**

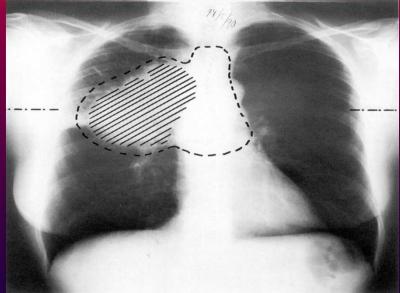
(The gross palpable or visible/demonstrable extent and location of the malignant growth)



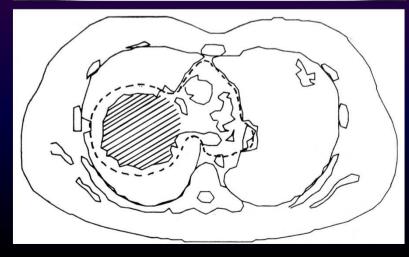
# **Clinical Target Volume (CTV)**

(A tissue volume that contains a GTV and/or subclinical microscopic malignant disease, which has to be eliminated)

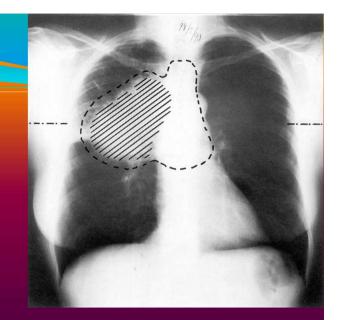




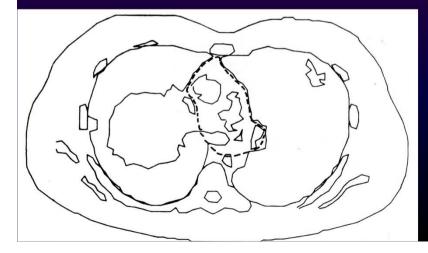


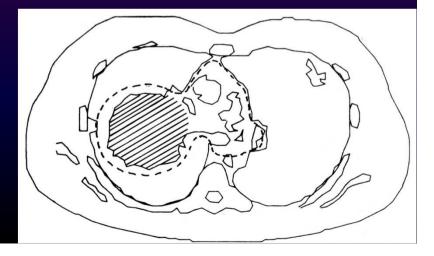






# The GTV & CTV concept is clear, but not easy to draw/delineate.





# Internal Target Volume (ITV)

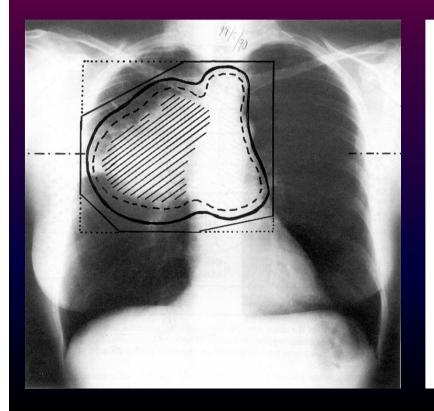
It is the CTV plus an internal margin. The internal margin is designed to take into account the variations in the size and position of the CTV relative to the patient's reference frame (usually defined by the bony anatomy); that is, variations due to organ motions such as breathing and bladder or rectal contents.

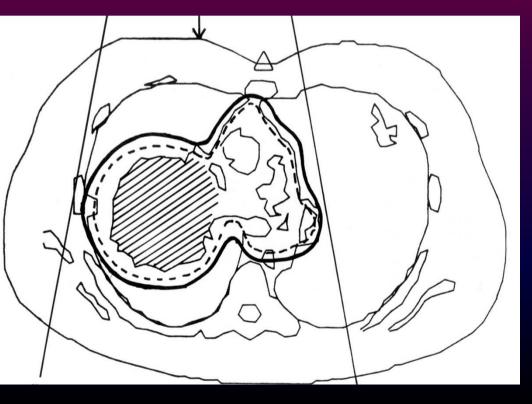
# **Organs at Risk**

Normal tissues, whose radiation sensitivity may significantly influence treatment planning and/or prescribed dose.

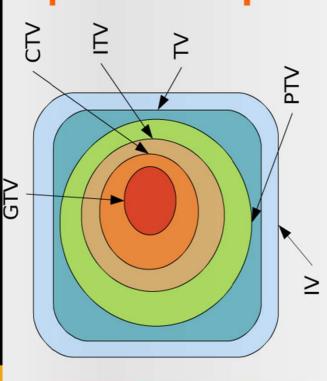
## **Planning Target Volume (PTV)**

(A geometrical concept that is defined to selcet appropriate beam sizes and beam arrangements, taking into consideration the net effect of all the possible geometrical variations and inaccuracies in order to ensure that the prescribed dose is actually absorbed in the CTV)





# Definitions: ICRU 50/62



- **Treated Volume**: Volume of the tumor and surrounding <u>normal</u> <u>tissue</u> that is included in the isodose surface representing the irradiation dose proposed for the treatment  $(V_{95})$
- **Irradiated Volume**: Volume included in an isodose surface with a <u>possible</u> biological impact on the <u>normal</u> tissue encompassed in this volume. Choice of isodose depends on the <u>biological end point</u> in mind.

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#### **Conformal Therapy**

Treatment plans create a high dose volume closely conforming to the shape of the PTV in 3D, and minimize dose to normal structures.

#### **Forward Planning**

• Define PTV-dose, Treatment Beams and Specify each beam parameters (*beam directions, weights, wedges, blocks, margins, etc.*)

Dose Calculation

 Assess dose distribution and adjust beam parameters until satisfactory plan is derived.

#### Intensity Modulated Radiation Therapy (IMRT)

Advanced image-guided 3D-CRT utilizing variable beam intensities determined via computerised optimization.

### **Inverse Planning**

 Clinical objectives (dose-volume constraints, Beam directions & dose distribution) specified in advance.

 Computerized optimization of pencil beam intensities (modulation) to best meet the desired dose constraints.

**Dynamic multileaf collimator (DMLC)** *MLC* is capable of dynamic leaf motion and sliding window. <u>Sliding-window</u> MLC leaves move continuously while the beam is on. The gap and speed for each opposing leaf pair modulates the dose. <u>Step & shoot in IMRT</u> Variable fluence across the field is created by summation of multiple static fields defined by MLC. For each static field, the MLC leaves are set (step), and a pre-calculated number of MU delivered (shoot).

The beam then halts, MLC shape changes, & the beam again comes on. The more steps, the finer gradation in fluence changes.

#### **Objective Function**

It is a mathematical description of criteria for treatment plan optimization that may be specified in terms of dose-limits, dose-volume limits, and/or in terms of dose-response functions etc.

#### <u>Score</u>

It is a numerical value of the objective function that represents a figure of merit, or quality of the treatment plan.

The best plan corresponds to the extremum-score.

#### Leaf motion file (leaf sequence file)

Data file generated by the TPS defines position of each MLC-leaf as a function of MU delivered.

It is then down-loaded to the MLC control computer on the accelerator for patient treatment.

#### <u>Autosequencing</u>

Accelerator control software that automatically sets up gantry, collimators, etc. for multi-field treatments. Particularly useful for `step and shoot' IMRT.



**IMRT & Inverse Treatment Planning (ITP)** 

• Objectives:

**Dose escalation Normal tissue dose sparing** 

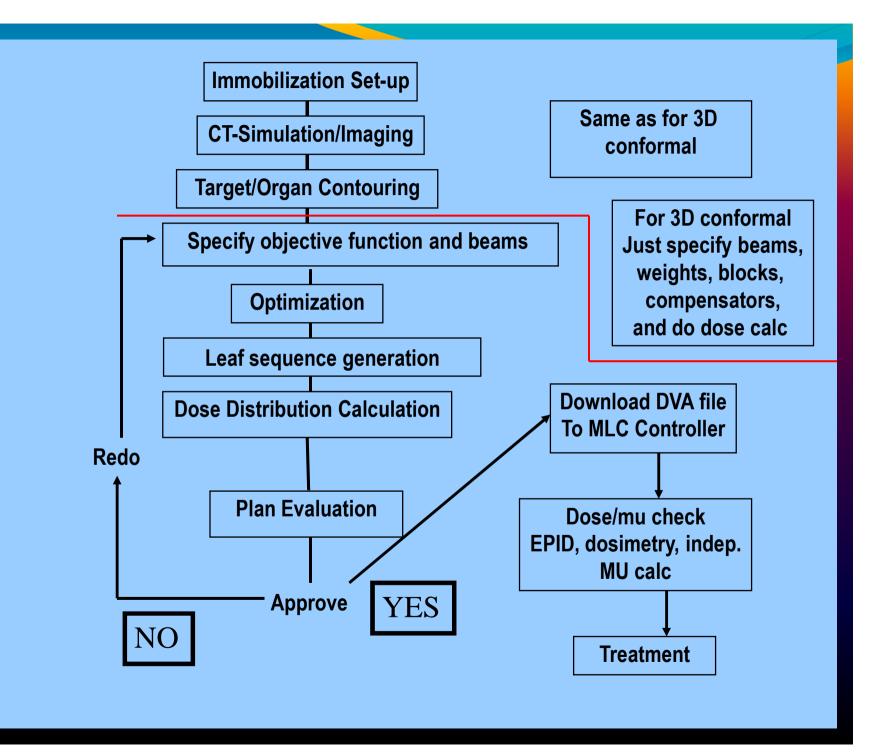
• Equipment Requirements:

MLC - DMLC ITP Computer System 3D-CT simulation Record and Verify system EPID Respiratory Gating System (for treatment and imaging)



# for

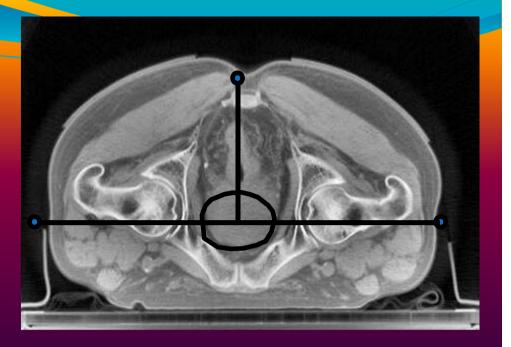
# **Treatment Planning**



#### **Tumor and**

#### **Tissue Contouring**

- 1. Isocenter defined at CT-Simulation
- 2. In room laser, skin marks, tatoos, etc.
- 3. Implanted markers?
- 4. Contour one or more GTV's.
- 5. GTV, CTV, PTV
- 6. Contour all normal tissues requiring dose volume constraints.



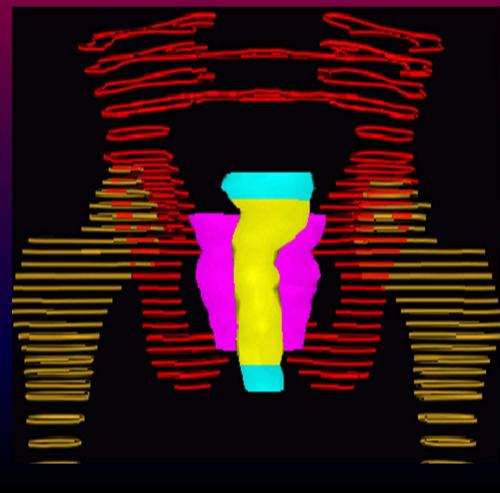


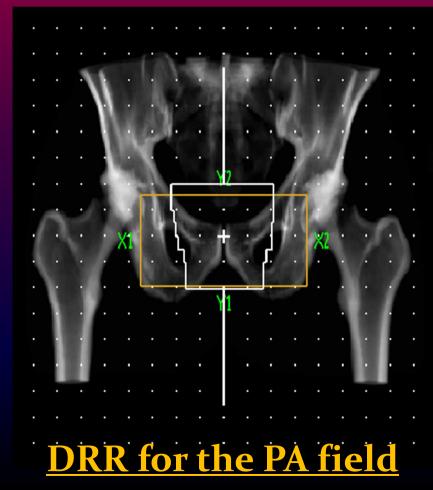
#### Example of IMRT contouring for Prostate + all relevant normal tissues

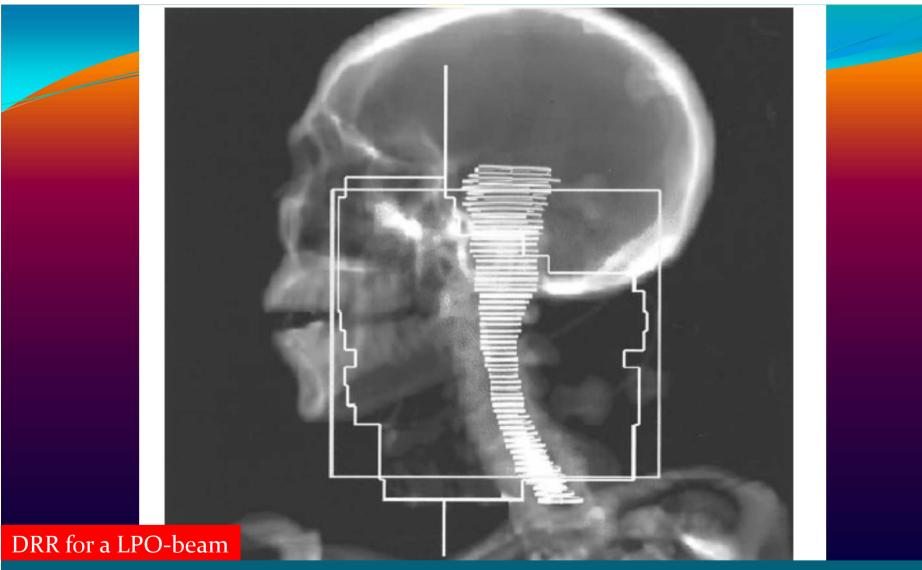
#### Length:

- Clinical / Conventional : one CT slice above & below PTV
- Anatomic

: anal verge to below sigmoid

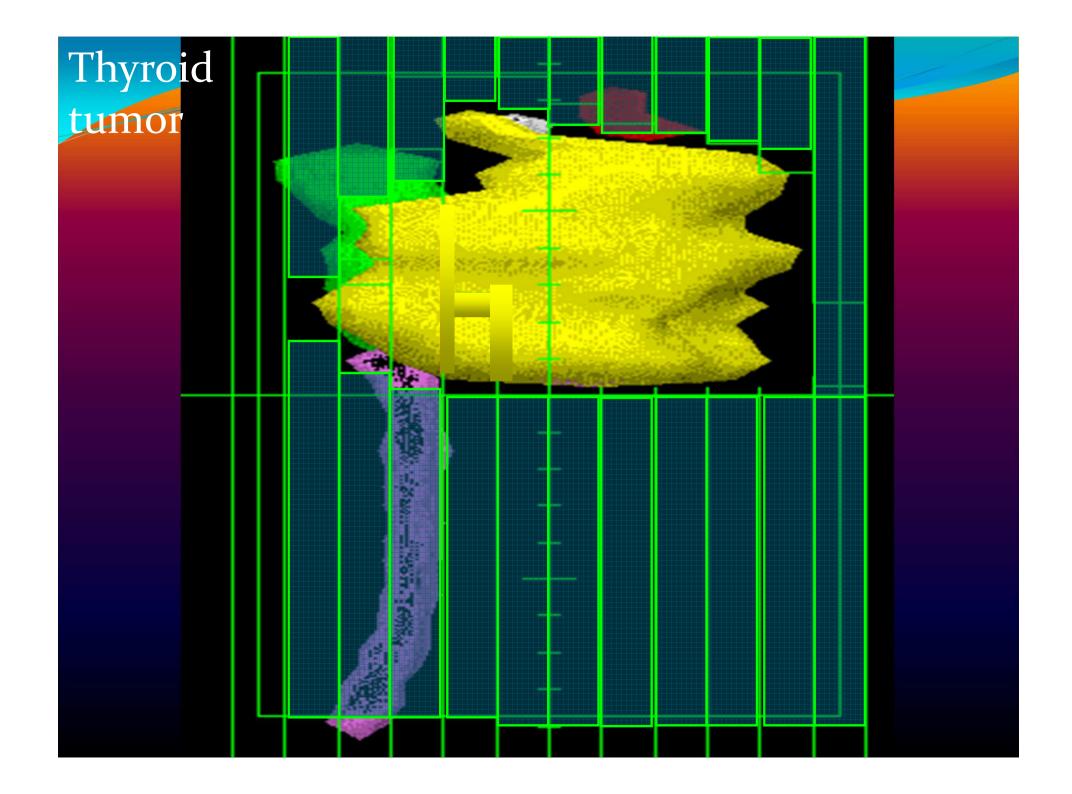




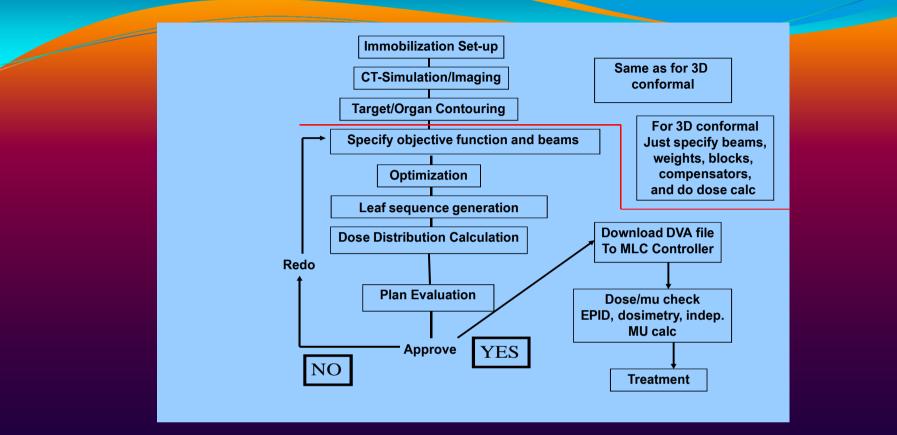


Initial wire-frame outlines of the spinal cord & Brainstem

> + Final DMLC-aperture







- Planner does NOT design blocks, choose wedges, assign beam weights, etc.
- Instead: Assign dose-volume constraints and penalties
- Plan-evaluation relies more on DVH
- Experience/ intuition from conventional planning not applicable to IMRT

#### **More differences**

- Hard to know if optimization succeeded or failed:
  - *a)* was objective function reasonable?
  - b) were dose-volume constraints achievable?
  - *c) stuck in local minimum?*
- Manual calculations to verify plans NOT POSSIBLE.
- *In-vivo* dosimetry, confirmation of beam delivery, and dose distributions more complicated.
- Only to trust your computers.
- Comprehensive QA-Program: Tailored to IMRT
- Factors usually inconsequential for conventional 3D-planning, become important with IMRT:
  - a) 2-3 times more monitor units: MLC leakage and scatter.
  - b) Room shielding design.
  - c) Patient whole body dose, neutron dose increase.
  - *d)* Longer treatment planning times (at least in the beginning).
  - e) Enormous volume of data transferred between computers.

#### How does the TPS find the optimum plan?

TPS doesn't really find the optimum plan.

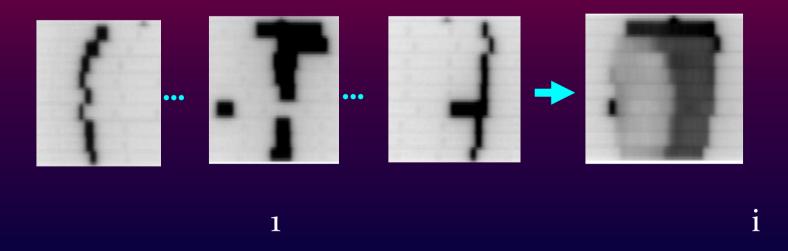
It finds a plan that best matches the dose volume constraints you specified.

So, if reasonably constraints are not provided to the TPS, we get a bad treatment plan.

Garbage in = Garbage out

# Delivery of IMRT with continuous leaf motion

- Each leaf pair forms a window which slides across the field.
- Dose given through the window as function of MU.



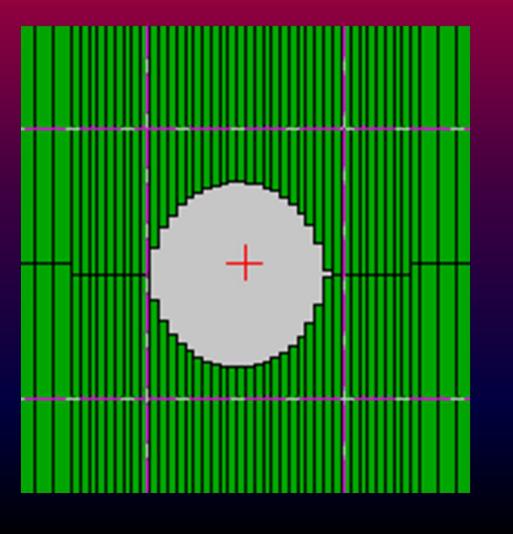
n 1+...+i+...+n
The final dose distribution is the summation from all segments.

# **Treatment Delivery (Summary)**

- IMRT fields can be delivered with dynamic (DMLC) or segmental (step-and-shoot) mode.
- It can be delivered (almost) any shaped intensity profile, subject to MLC limitations and beam properties.
- It needs account for leaf transmission, rounded leaf end and head scatter, leaf speed, etc.
- Large fields may have to be split into 2 or 3 sub-fields.
- Loss of beam-on time efficiency relative to conventional fields due to small field openings.

# **3D-CRT fields**

#### Tracking a tumor moving with respiratory motion

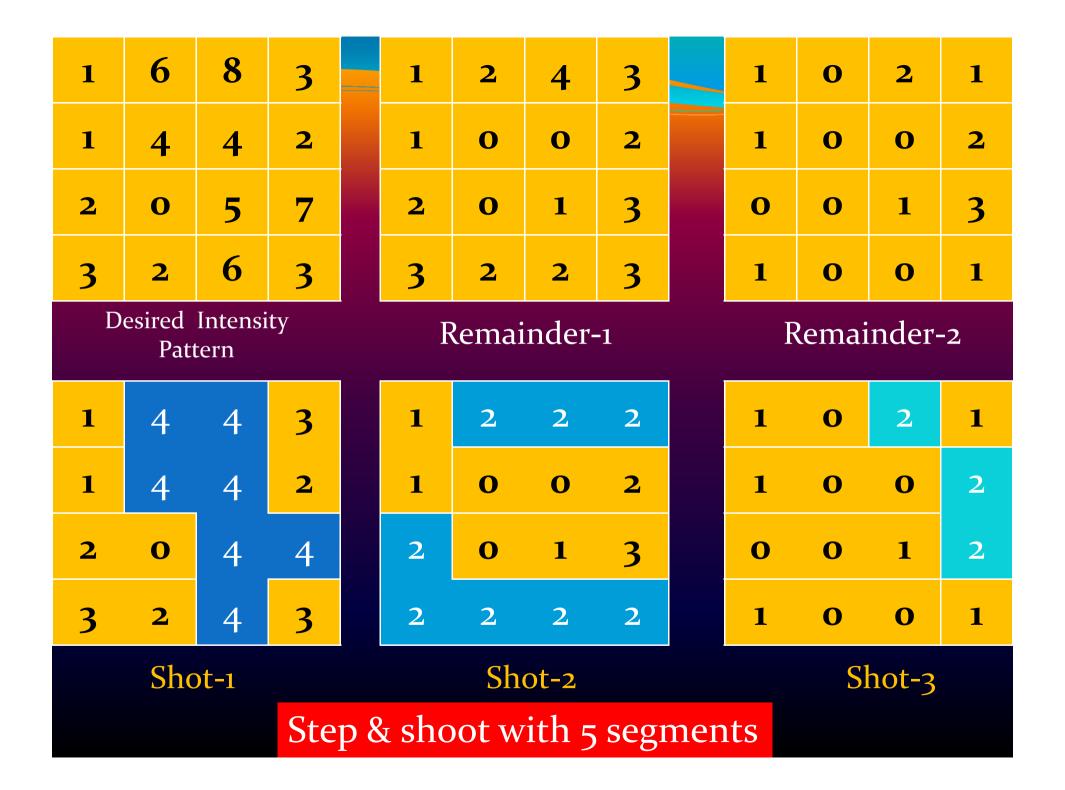




# **DMLC-IMRT fields**

# With NO-motion compensation

#### Tracking a tumor moving with respiratory motion



1 1 0	0 0 0	2 0 1	1 2 3		1 1 0	0 0 0	0 0 1	1 0 1	2	Step & shoot with 5 segments			
1	0	0	1		1	0	0	1	0	0	0	1	
R	Remainder-2 Remainder-3						0	0	0	0			
1	0	2	1		1	0	0	1	0	0	Ο	0	
1	0	0	2		1	0	0	0	Ο	0	Ο	1	
0	0	1	2		Ο	0	1	1	Remainder-4 & Shot-5				
1	Ο	Ο	1		1	0	Ο	1					
Shot-3 Shot-4													

How to fix an IMRT plan that doesn't meet constraints

Integral dose =  $\int d_v \, dV$  is a constant, dependents only on patient shape, prescription dose, and number of beams selected

Think of it as a balloon. Squeeze in some place and it pops out some place else..

# Ask for more than you want?

- Solutions are a "compromise"
- Objectives are "penalty" based (no rewards)
- Lenient constraints may lead to miss a better solution

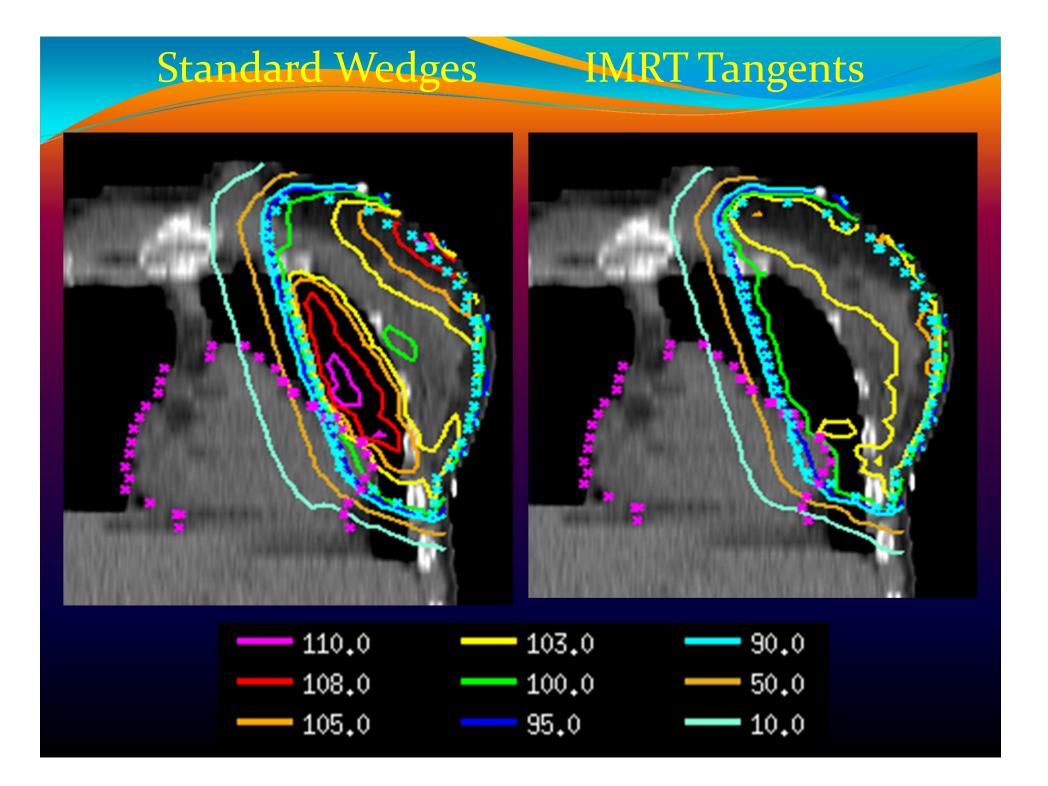
# IMRT for Breast instead of Wedges

IMRT tangents can

• Improve target dose homogeneity

• Modestly reduce dose to ipsi-lateral lung and heart

• Reduce dose to contra-lateral breast



#### **Treatment Planning Issues for Lung**

- GTVs and especially CTVs difficult to define without CT+PET
- Normal lung surrounds PTV (Radiation Pneumonitis)
- Setup uncertainties
- Respiratory motion
- Methods to reduce breathing motion:
  - Respiratory gating
  - Breath-hold: voluntary/forced

