

## Conventional Brachytherapy In Carcinoma Cervix. A HISTORICAL PERSPECTIVE

Dr. RAKESH KAPOOR

MD, MAMS, FICRO

**Professor & Head Unit II** 

Department of Radiotherapy and clinical Oncology, Tertiary Cancer Center, PGIMER Chairman Indian College Of Radiation Oncology.

Founder Director HBCH & RC Punjab. (Unit of T.M.C, Mumbai) DAE,(GOI)

Ex. Head: Department of Biostatistics, P.G.I.M.E.R Ex. Additional Medical Superintendent, P.G.I.M.E.R

# BRACHYTHERAPY

- Brachy
  - Short distance (Greek)
- Brachytherapy is a type of radiation treatment in which small, encapsulated radioactive sources are arranged in a geometric fashion in & around tumor.
- ADV.
  - It delivers very high dose of radiation to tumor
  - Sparing normal tissue
  - Dose delivered in short duration as compared to External beam RT.
- Cavity
  - Hollow space within the body.
  - Lumen cavity within a tubular organ.
- Intracavitary brachytherapy
  - Gynecological sites cervix, uterus, vagina.

# **Anatomy & Pathology**

- Relationship of uterus & vagina
  - Uterus is usually anteverted & anteflexed and it lies at right angles to the vagina.
    - Construction of applicator.
- Relationship of rectum & bladder
  - Important consideration regarding the dose received by brachytherapy complications
- Spread of disease
  - Predominant line of spread laterally thru paracervical tissues into parametrium
  - Into uterus & vagina
  - Only in very advanced into bladder & rectum
  - Brachytherapy doses should reach more laterally than anteroposteriorly

## **Types of IC brachytherapy**

#### • Depending upon loading technology

- Preloaded radium tubes
- After loaded
  - Manual Cs <sup>137</sup>
  - Remote  $Cs^{137}$ ,  $Co^{60}$ ,  $Ir^{192}$ .
- Based on dose rates used
  - Low dose rate LDR
    - 0.4-2 Gy/ hr
    - Ra <sup>226</sup>, Cs <sup>137</sup>
  - Medium dose rate MDR
    - 2-12 Gy/hr
    - Cs <sup>137</sup>
    - In PGI we consider, any dose rate > 0.9 Gy/hr which require dose rate correction as MDR.
  - High dose rate HDR
    - > 12 Gy/hr
    - Co<sup>60</sup>, Ir<sup>192</sup>

## WHY I/C BRACHYTHERAPY

- Optimal conformal dose delivery system.
- Inhomogeneous dose very high dose locally, rapid fall off.
  - Cervix receives 20,000 25000 cGys.
  - Uterus receives 20,000- 30000 cGys.
  - Vagina receives 10,000 cGys.

such high doses can't be delivered by any technique of EBRT.

- Sparing of early & late responding normal tissues.
- Short overall treatment time
- Counter tumor repopulation.
- Best long-term control is achieved
- Less late radiation morbidity .
- Preservation of normal anatomy.
- Better sexual functional life.

# **BRACHYTHERAPY in Cervix**

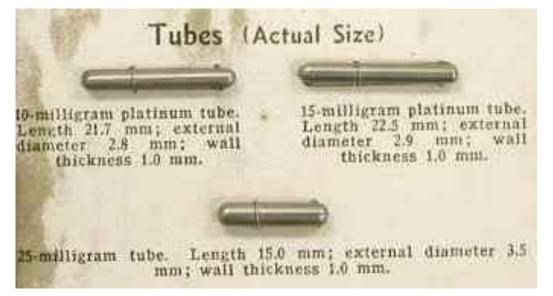
- Brachytherapy plays vital role in treatment of ca cx. & is mainly applied as an intracavitary procedure in selected cases complemented by interstitial implants.
- **Cervical cancer** is an ideal site for I/C brachytherapy because
  - High tolerance of cervix ,uterus & vagina
  - It is accessible organ hence Brachytherapy can be practiced with ease.
  - The endocervical canal & vaginal vault form a suitable vehicle to carry rigid applicators with radioactive sources.
  - These applicators can be used with minor modifications in all pts.
- I/C applications are temporary that are left in the patient for a specified time to deliver prescribed dose.

# HISTORY

- 1898: Discovery of Radium by Marie Curie in Paris.
- 1903: Margaret Cleaves, a New York physician described inserting Radium into the Uterine cavity of a patient with Ca Cervix.
- 1908: I/C brachytherapy started in Vienna
- 1910: I/C brachytherapy started in Stockholm
- 1912: I/C brachytherapy started at Paris.
- 1930: Todd & Meredith developed Manchester system in U.K.
- 1960s: After loading technique (Helneski)
- 1970: Paris System of dosimetry for Interstitial Brachytherapy evolved
- 1975: Remote Control LDR (Cs-137)
- 1985: -HDR Introduces(Ir-192 & Co-60) & ICRU-38 Published
  - -Concept of Volume in place of point introduced
  - -Joshlin Published data about the discrepancies in point A & B
- 1990s: Miniaturized stepping source with optimization

# SOURCES

- Radium 226 LDR
  - As tubes, with 1 mm platinum filtration.
  - Avg energy -0.83 MeV
  - Half life 1626 yrs.
- Cobalt 60 HDR
  - High dose rate system
    - Pellets similar to Cs137.
    - Higher activity 500 mCi/pellet
- Iridium 192 HDR
  - Active wire (dia -0.2-1.3 mm, AL 1-20 mm)
    - Nucletron 1.1 mm, 4 mm
  - Encased in stainless steel
  - Permanently attached to cable drive.
  - Activity 10 Ci (370 GBq)





- Cesium 137 LDR/MDR
  - Manual after loading.
    - Miniature cylindrical sealed sources 5x1.8 mm.
    - Active bead 1.1 mm diameter
    - Spherical steel spacers 1.8 mm
  - Remote after loading
    - Incorporated into glass bead -1.5 mm diameter
    - Encapsulated stainless steel ball bearing 2.5 mm diameter.
    - Activity 40 mCi/pellet
  - Preloaded
    - In forms of tubes, similar to radium
    - 25 mg (TL-2 cm, AL-1.35 cm, Dia- 4.05 mm)
    - 20 mg (same dimensions)

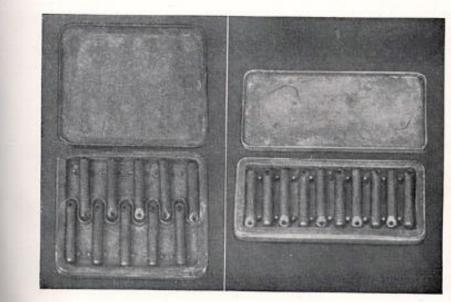
## **DOSIMETRIC SYSTEMS**

- The historical dosimetric systems were developed when computer treatment planning and dose computations were not available
- Term 'system' specifies a set of rules for
  - Geometrical arrangement of a specific set of radio isotopes in a specialized applicator
  - To obtain suitable dose distributions over the volume to be treated.
  - It specifies treatment in terms of the dose, time and administration
  - A specified set of tables to allow, reproducible and easy calculation in most of the encountered clinical scenarios.
  - A system ensures safety and is based on clinical experience.

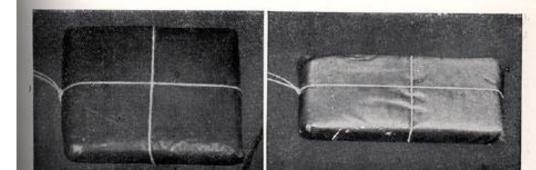
# **STOCKHOLM SYSTEM**

- Work of Forsell at radium hemmet -1910
  - Unequal amounts of radium used.
    - Uterus 30-90 mg in rigid tube
    - Vagina 60-80 mg in shielded lead/silver boxes
    - Vaginal & uterine applicators not fixed
- Fractionated (2-3 #s) course over a period of one month.
- Heavy doses for a period of 20-30 hours each.
- Separated by 1-3wks
- This system used
  - Intravaginal boxes made up of silver or gold
  - The intrauterine tube made up of flexible rubber.
  - These were not fixed together

Figs. 7 and 8. Flat applicators of various types for vaginal application. Full size. The property of Radiumhemmet.



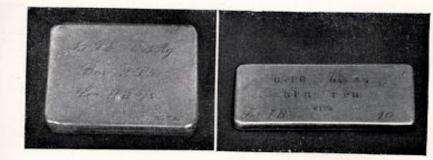
Figs, 9 and 10. The same applicators with their tubes.



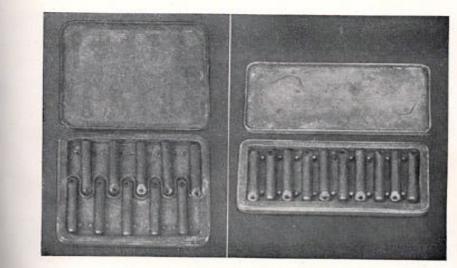
Unequal amounts of radium used.
Uterus – 30-90mg in rigid tube
Vagina – 60-80mg in shielded lead/silver boxes
Vaginal & uterine applicators –not fixed

Heavy doses, each lasting 20-30hrs
6500 – 7100 mg hrs.

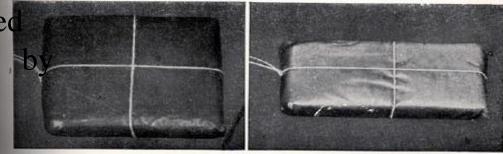
- •Results -1914-25 (5 yr results)
- •Treated -1455
- •Symptom free -327
- •Cure rate 22.5%
- A total dose of 6500 -7100 mg -hrs was prescribed out of which 4500 mg Ra was contributed the vaginalbox. (dose rate-110R/hr)



Figs. 7 and 8. Flat applicators of various types for vaginal application. Full size. The property of Radiumhemmet.



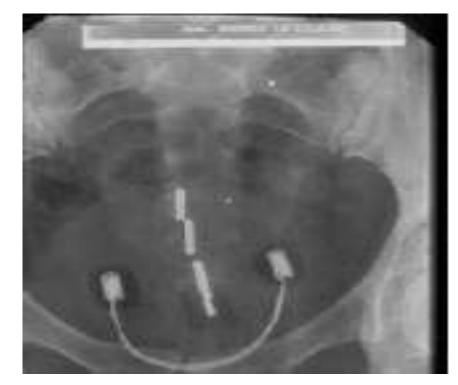
Figs, 9 and 10. The same applicators with their tubes.



# PARIS SYSTEM

- Regaud, 1919, Institute of radium, Paris
- Single application of Radium for 120 hrs (5-6days)
- Designed to deliver a dose of 7000 8000 mg/hrs over a period of 5 days (45 R/hr) (5500 mg/hr)
- In this system, almost an equal amount of Radium was used in the uterus and the vagina.
- The system incorporated
  - Two cork colpostats (cylinder) with 13.3mg Radium in each
  - An intrauterine tube of silk rubber with 33.3mg Radium
- The intrauterine sources contained three radioactive sources, with source strengths in the ratio of 1:1:0.5





- •Regaud, 1919, Institute of radium, Paris
- •Fixed mg-hrs for a specified tumor volume.
- •Smaller amounts of radium for longer time.
- •Uterus 6.6+13.33+13.33 mg Ra rubber tubes
- •Vagina 13.33 in each cork colpostats.
- •Time: 120 hrs
- •7200-8000 mg hrs.
- •Initially colpostats alone  $\rightarrow$  colpostats+ tandem  $\rightarrow$  tandem alone.
- •Results 1923
  - Symptom free survival -43.9%

Designed to deliver a dose of 7000 - 8000 mg hrs over a period of 5days (45R/hr) (5500mg/hr)



### FALLACIES

- Long treatment time, discomfort to the patient
- Dose prescription method was empirical. Both systems specified dose in mg-hour.
- Does not give any information about dose distribution.
- When used in conjunction with EBRT, overall radiation treatment can't be adequately defined
- Dose specification method lacks the information on
  - Source arrangement
  - Position of tandem relative to the ovoids
  - Packing of the applicators
  - Tumour size, and
  - Patient anatomy.
- With the use of this dose prescription method dose to important anatomical targets could not be quantified adequately.
- Ignored the importance of tolerance of different critical organs to radiation.

### DOSE SPECIFICATION

- Done in mg-hr i.e. simple mathematical product of mg of Radium times the duration (in hours) of the implant.
- It was easy to use.
- The dose prescription was entirely empirical due to the lack of
  - knowledge about the biological effects of radiation on the normal tissues and the tumor
  - understanding about the dose, dose distribution and the duration of treatment.
  - Only applicable when both tandem & ovoids are used & sources are loaded in a rigidly prescribed manner.

## MANCHESTER SYSTEM

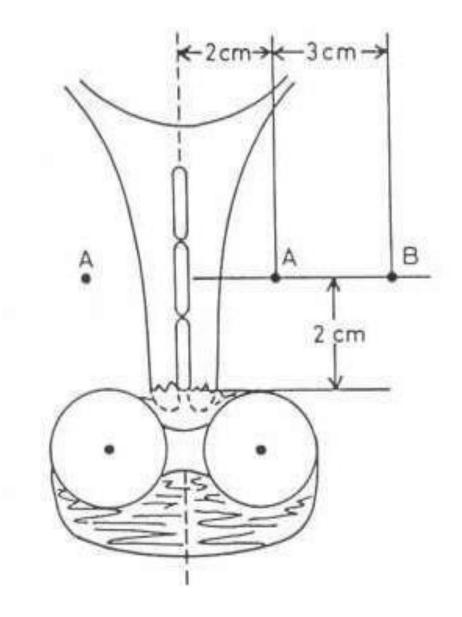
- The Manchester system is one of the oldest & extensively used systems in the world.
- Developed by Todd & Meredith in 1930 & was in clinical use by 1932.
- This system was initially developed for radium tubes but was easily adapted to different afterloading systems.
- Predetermined doses & dose rates to reduce the empirism & high complication rates.
- Dose specified at fixed points point A
- Specified therapy in terms of absorbed dose Roentgen instead of mg hrs.
- Initially preloaded  $\rightarrow$  manual after loaded  $\rightarrow$  remote after loaded.
- Initially for LDR. Now used for MDR & HDR also.

Manchester system was based on following principles:

- To define the treatment in terms of dose to a point
  - It should be anatomically comparable from patient to patient.
  - Should be in a region where the dosage is not highly sensitive to small alteration in applicator position.
  - Should be in position that allows correlation of dose with clinical effects
- To design a set of applicators and their loading (with a given amount of radium), which would give the same dose rate irrespective of the combination of applicators used.
- To formulate a set of rules regarding the activity, relationship & positioning of the radium sources in the tandem & vaginal ovoids to achieve desired dose rate.

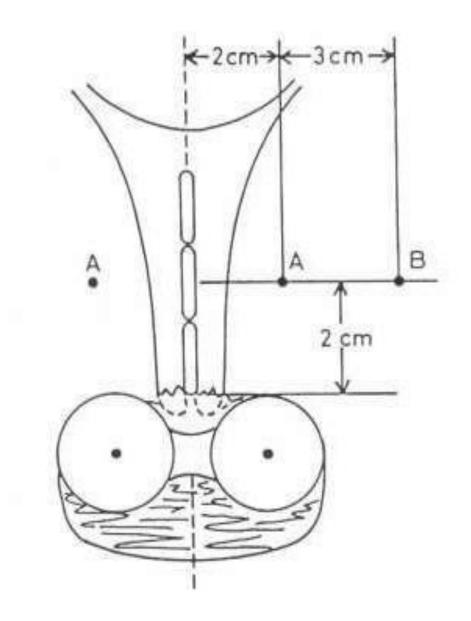
#### POINTA

- Todd & Meredith defined a point in paracervical triangle where the uterine vessels cross the ureter as point A.
- Point A, lies in the paracervical triangle.
- Point A is defined as a point 2 cm. lateral to the center of the uterine canal and 2 cm. superior to the mucosa of the lateral fornix, in the plane of the uterus.
- Now point A is defined as a point 2 cm above the distal end of lowest source in cervical canal & 2 cm lateral to centre of tandem.
- ABS recommends this point as it falls within the portion of the isodose distribution with little cephalocaudal gradient.



### POINT B

- To know the rate of fall of dose external to point A, as an index to the volume of tissue treated.
- Quantifies the dose delivered to the obturator lymph nodes.
- Point B is defined 2cm above external os & 5 cm laterally to midline.
- Represents dose to the pelvic wall, obturator L.N.
- The dose at point B is approx. 25 -30% of the dose at point A.
- Dose to point B, depends little on the geometric distribution of radium, but on the total amount of radium used.



### DOSE LIMITING STRUCTURES

- Bladder
- Rectum
- Vaginal mucosa
- Rectovaginal septum
  - No more than 40% of total dose at point A could be delivered safely through the vaginal mucosa.
  - The rectal dose should be 80% or less of the dose at point A; this rectal dose can usually be achieved by careful packing.

#### APPICATOR IN MANCHESTER SYSTEM

- Similar to those used in Paris system
- It had a pair of ovoids & an intrauterine tube
  - Intrauterine applicator
    - Rubber tubing, with flange at end.
    - Varying length, can take 1,2,3 radium tubes in line.
  - Ovoids
    - Rubber or nylon
    - Shape follows the distribution in 3-D space of the isodose curves around the contained radium tube, ensuring homogenous dose on its surface.



#### INTRAUTERINE TUBE

- The intrauterine tube was made up of the thin rubber (to prevent excessive dilatation of the cervical canal)
- These tubes were available in three separate lengths
  - 2cm
  - 4cm
  - 6ст
- In order to accommodate 1, 2 or three Radium tubes (2 cm long) in line I.U.tubes were closed at one end, and had a flange at the other end so that when packed into position, the uterine tube did not slip out during the treatment.



#### **OVOIDS**

- Used in pairs, one in each lateral fornix
- The shape of ovoids mimics the shape of isodose curves around a Radium tube having "active length" of 1.5 cm.
- The ovoids were designed to be adaptable to the different vaginal capacity, with diameter of 3 sizes
  - Small dia = 2 cm
  - Medium dia = 2.5 cm
  - Large dia –=3 cm.
- *"WASHER"* holds the ovoids in position in narrow vagina.
- The largest ovoid are placed in the roomiest vagina in order to achieve the best lateral dose throw off



#### SPACERS

- Apart from ovoids & I.U.tubes spacers or washers were used
  - To maintain the distance between the ovoids
  - To help in their fixation
- Pairs of ovoids held apart by a "*SPACER*" rubber.
  - Fixes at a distance of 1 cm.
- Spacer was used to give the largest possible separation b/w the ovoids so that the dose could be carried out as far laterally as possible.
- It maintained a distance of 1cm b/w the ovoids.



#### PACKING

- Manchester applicators do not incorporate rectal shielding.
- Hence gauze is packed firmly and carefully
  - behind the ovoids,
  - anteriorly b/w the ovoids and the base of the bladder,
  - and around the applicator tubes down to the level of the introitus
- Packing helps to
  - keep the applicators in position
  - to reduce dose to bladder and anterior rectal wall.

### RULES

- The point A should receive the same dose rate, irrespective of the combination of applicators used.
- Not more than one third of the total dose to point A should be delivered by the vaginal ovoids. So that tolerance of vagina mucosa is not exceeded.
- Standard or ideal loading is 60-40 i.e. 60% of the dose to point A is contributed by intrauterine sources while 40% is contributed by ovoids.
- Total Dose to point A : 8000 R
  - Total number of applications : 2
  - Total time for each application : 72 hrs
  - Total time : 144 hrs
  - Dose rate desired : 55.5 R /hour to point A
- Amount of radium to be used was defined in terms of units.
- 1 unit = 2.5 mg of radium filtered by 1 mm platinum.
- The loadings were specified in terms of integral multiples of this unit.

## LOADING PATTERN

- Total dose at point A using different combinations of IU tube & ovoids :
  - Large tube with large ovoid and washer : 57.5 R
  - Large tube with large ovoid and spacer: 56.9 R
  - Large tube with small ovoid and washer: 57.6 R
  - Medium tube with small ovoids and spacer: 57.3 R
- The variations were thus within 1.5% range.

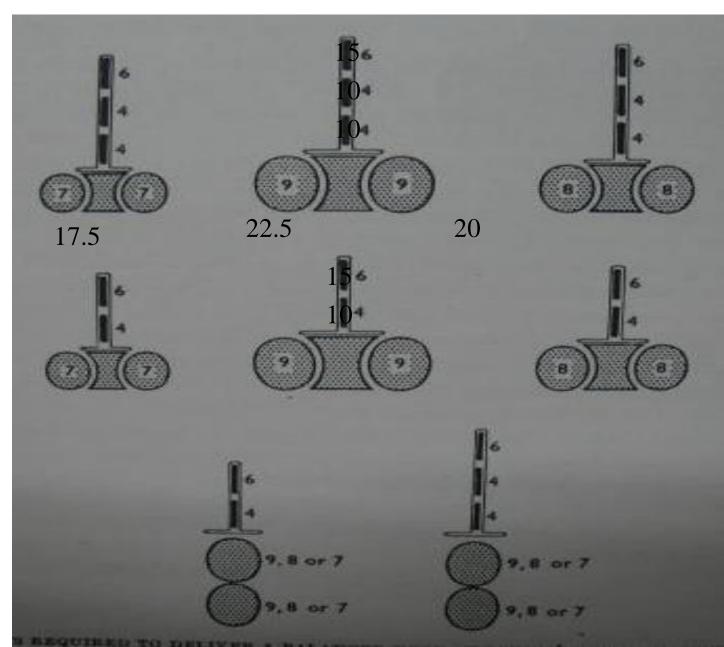
#### Using 2.5 mg

# Loading pattern

1 unit = 2.0/2.5/3.33 mg

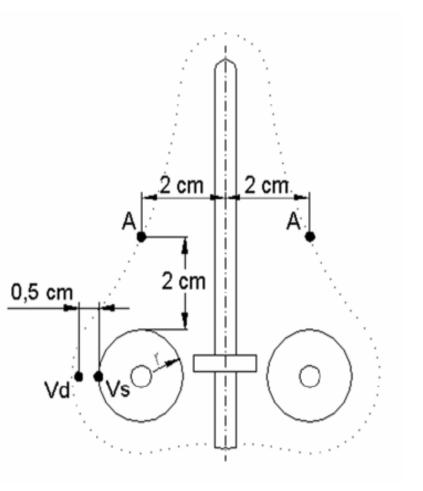
- Unit dose A dose B 2mg 1000r large – 39%
- 2.5 1366r medium 33%
- 3.33 1820r small 29%

Per 24 hrs.



# Loading pattern

- Vaginal contribution to point A 40% only.
- Point B dose ~ 9 Gy for every 4000 mg hr.
- Depending upon loading, could deliver from 8400 11200 mg hr.
- Dose prescribed 8000r (72.8Gy) to point A in 2 applications.
  - 70 hrs if 2.5 mg unit.



- Preloaded LDR system.
  - Flexible, loose system- can be inserted even if cervix distorted.
  - Cheap and durable
  - Good geometry attained in experienced hands.
  - Decades of experience
  - Not fixed, high chance of improper geometry, slippage of application.
  - Radiation hazard.
- Preloaded LDR system
  - cesium 137 tubes
- Manual after loaded system
  - Cesium 137, Cobalt 60
    - Reduced radiation hazard.
    - Better application possible.
    - Retains application in position better.

- Remote after loading system.
  - Initially sources as tubes unpopular –mechanical problems
  - Sources as pellets 1975 nucletron.
- Classical LDR 53cGy/hr
- Modern system 140 180 cGy/hr
  - Initially dose rate correction factor not applied.
  - Higher complication rates.
  - Fowler etal 75cGy/hr 150cGy/hr grade 2&3 12% 32% grade 3 4% 22%

Inspite of 20 % reduction of dose.

## **ICRU SYSTEM**

- For reliable and relevant comparison of different methods and their clinical results ICRU 38 recommends a common terminology for prescribing recording and reporting I/C Brachytherapy applications.
- The ICRU recommends a system of dose specification that relates the dose distribution to the target volume, instead of the dose to a specific point
- The dose is prescribed as the value of an isodose surface that just surrounds the target volume.
- ICRU Reporting
  - Description of technique
  - Dose at reference points
  - Description of reference volume

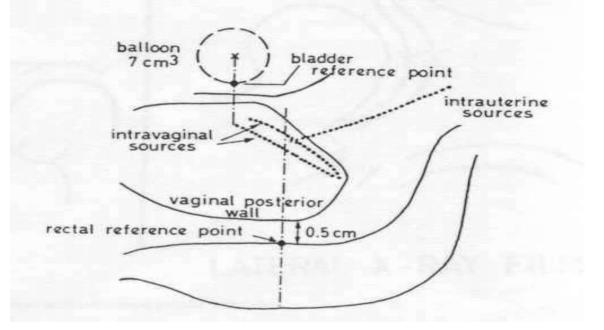
#### Description of the Technique

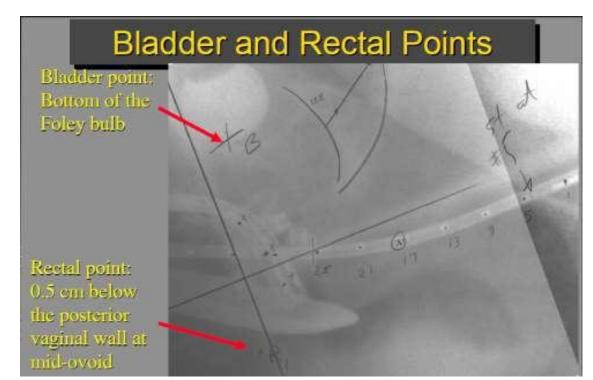
- Minimum information should include the
  - orthogonal radiographs of the application.
  - Source used (radionuclide, shape and size of source, and filtration)
  - applicator type
  - Loading pattern
  - Simulation of linear source for point or moving sources
  - Applicator geometry (rigidity, tandem curvature, vaginal uterine connection, source geometry, shielding material)

#### Dose at Reference points

#### BLADDER POINT

- ICRU recommends:
  - Foley balloon filled with 7cc of radiopaque fluid and pulled down against urethra
  - On lateral radiograph reporting dose at a point at posterior surface of Foley balloon on AP line through centre of balloon.
  - On AP radiograph, reference point is taken at the centre of the balloon

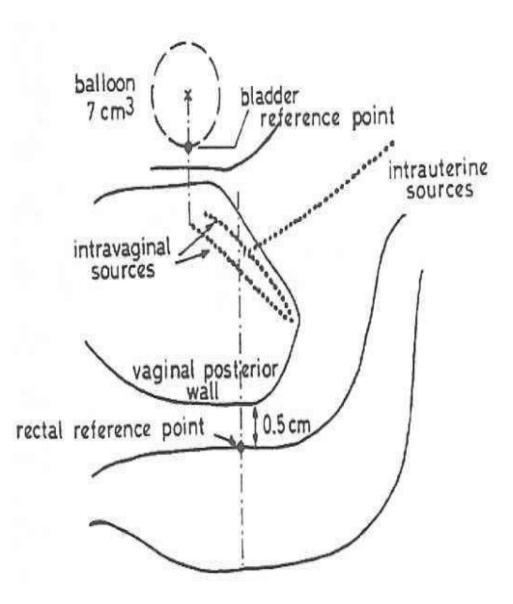




#### **RECTAL POINT**

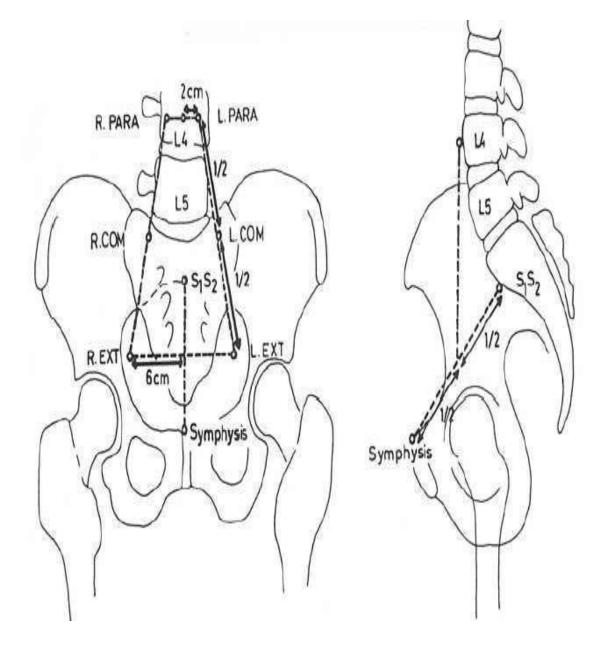
#### • ICRU recommends:

- The dose is calculated at a point 5 mm posterior to (opacified) vaginal cavity along an AP line midway between vaginal sources.
- On the frontal radiograph, this reference point is taken at the intersection of (the lower end of) the intrauterine source through the plane of the vaginal sources



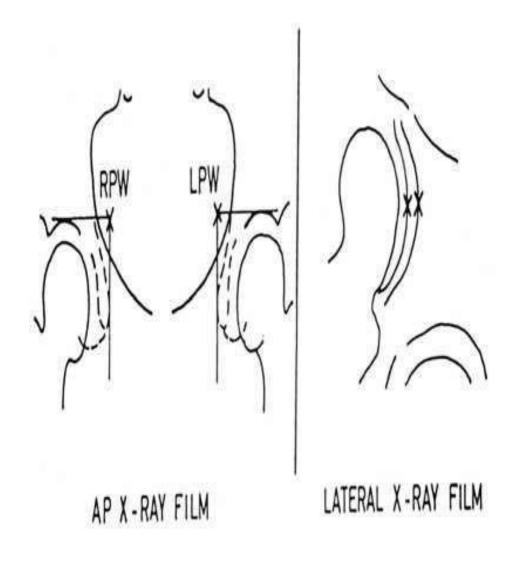
#### LYMPHATIC TRAPIZOID

- Lymphatic trapezoid represents dose at lower Para-aortic, common and external iliac L.N.
- A line is drawn from S1-S2 junction to top of symphysis, then a line is drawn from middle of this line to middle of ant. aspect of L4.
- A trapezoid is constructed in a plane passing through transverse line in pelvic brim plane and midpoint of ant. aspect of body of L4.



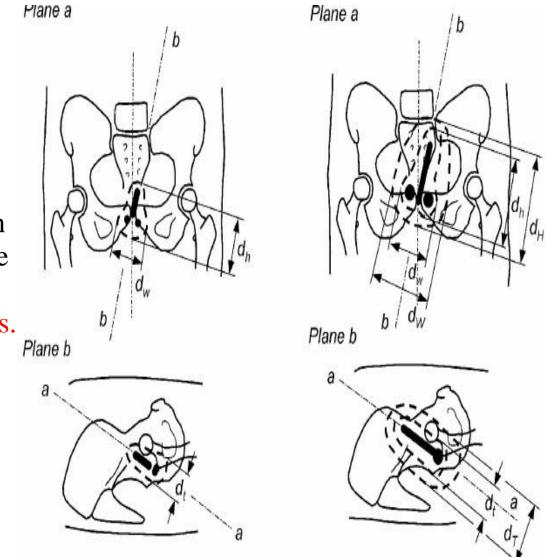
#### PELVIC WALL REFERENCE POINTS

- The pelvic wall reference point, represents absorbed dose at the distal part of the parametrium and at the obturator L.N.
- On anAP radiograph, pelvic-wall reference point is located at intersection of following lines
  - •A horizontal line tangential to the highest point of the acetabulum,
  - •A vertical line tangential to the inner aspect of the acetabulum.
- On a lateral radiograph, the highest points of the right & left acetabulum, in craniocaudal direction, are joined & lateral projection of the pelvic-wall reference point is located mid-way b/w these points.



### Description of Reference volume

- Volume encompassed by the reference isodose, selected and specified to compare treatments performed in different centres using different techniques.
- ICRU (43) recommends reference volume be taken the as the 60-Gy isodose surface, resulting from the addition of dose contributions from any externalbeam whole-pelvis irradiation and all I/C insertions.
  - Height 'h'
  - Width 'w'
  - Thickness 't'.
  - and *their product* should be reported separately



- Treated Volume
  - The Treated Volume is the pear and banana shape volume that received (at least) the dose selected and specified by the radiation oncologist to achieve the purpose of the treatment e.g., tumour eradication or palliation, within the limits of acceptable complications.
- Irradiated Volume
  - The irradiated volume is the volume, surrounding the treated volume, encompassed by a lower isodose to be specified, e.g., 90 50% of the dose defining the treated volume.
  - Reporting irradiated volumes is useful for interpretation of side effects outside the treated volume and for purpose of comparison

# HIGH DOSE RATE

- After loading systems.
  - Developed in 1968 by Joslin
  - Initially Cobalt 60, now iridium 192.
- BED calculation of equivalence
  - Based on LQ model
- For equivalence to LDR the dose/# needs to be  $\sim$ 3 Gy.
- However, this based on the t1/2 of late reacting tissues -1.5 hrs.
- If assumed to be 4 hrs., then dose/# be 6-12 Gy and HDR may be radio biologically better.
- Also, better geometrical sparing due to better packing away of critical organs

For HDR: BED = 
$$Nd\left(1 + \frac{d}{\alpha/\beta}\right)$$

For LDR: BED = NRt 
$$\left[1 + \frac{2R}{\mu(\alpha/\beta)} \left\{1 - \frac{1 - e^{-\mu t}}{\mu t}\right\}\right]$$

## Advantages of HDR

- 1. Shorter treatment times, resulting in:
  - Less patient discomfort since prolonged bed rest is eliminated .
  - Reduced applicator movement during therapy.
  - Greater displacement of nearby normal tissues.
  - Possibility of treating larger number of patients.
- 2. Allows use of smaller diameter sources than are used in HDR:
  - Reducing the need for heavy sedation or general anesthesia (allowing treatment for high-risk patients who are unable to tolerate general anesthesia).
  - Making insertion of the tandem into the cervix easier.
- 3. Tailor dose distribution to target through optimization.
- 4. Elimination of exposure to personnel.

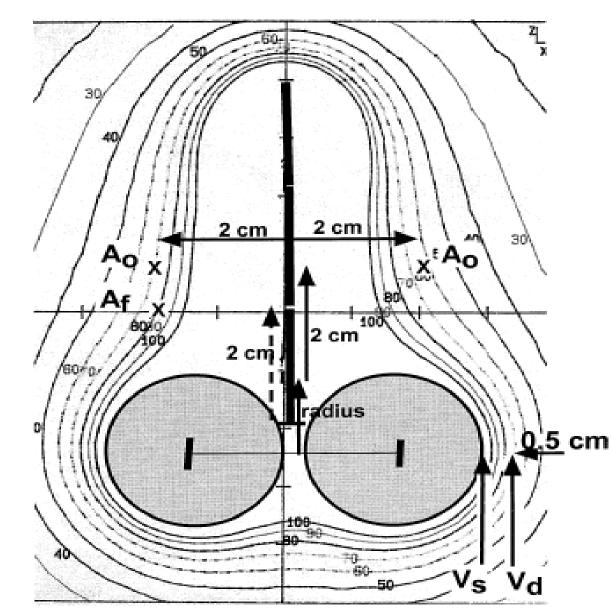
## Disadvantages of HDR

- 1. Labor intensive (requires large staff during procedure)
- 2. Decreased therapeutic ratio (radio biologically, normal tissue becomes relatively more sensitive than tumor)
- 3. Increased probability of executing an error
- 4. Must know target and desired doses
- 5. Repeated multiple times different geometry each time.

# **ABS RECOMMENDATIONS**

#### **ABS recommendation for locating point A**

- From the point of intersection of the line connecting middle of both the ovoids with the central tandem, move superiorly along the tandem, 2cm + radius of the colpostats & then 2cm perpendicular to the tandem in the lateral direction.
- Dose reporting
  - Lateral vaginal surface V<sub>s</sub>
  - 0.5 cm deep to vaginal surface  $V_d$
  - Limit Vs dose to <150% of point A dose.
  - Nominal bladder point-ICRU 38
  - Nominal rectal point ICRU 38
  - Keep bladder dose < 80Gy\*
  - Rectal dose < 75 Gy\*
  - Pelvic wall point ICRU 38



## **ABS recommendation for LDR**

- Procedure under analgesia/ anesthesia
- Use of 2 LDR applications in larger tumors (single if unreliable patient, excellent geometry, small tumor)
- Entire Rx completed in 8 wks.
- Place radio-opaque markers on cervix to determine relation of vaginal applicators to cervix.
- Use largest colpostat accommodated.
- Ideally tandem bisects the colpostat on lateral view & tandem falls midway b/w colpostats & parallel to body axis on AP view.
- 7cc foley's bulb

#### Suggested doses for LDR brachytherapy

Table 2. Carcinoma of the uterine cervix: Suggested doses of external beam irradiation and LDR intracavitary brachytherapy\*

		External irradiation (Gy)		LDR brachytherapy (Gy)		
Tumor stage	Tumor extent	Whole pelvis	Pelvic wall	Parametrial boost (Gy)	Dose to point A	Total dose to point A (Gy)
IA1		0	0	0	50-60	50-60
IA2 Selected IB1	Superficial ulceration less than 1 cm in diameter or involving					
	fewer than two quadrants	0	0	0	60–70	60-70
IB1	-	19.8 or 45	50.4 or 45	0	55 or 30–35	75 or 75–80
IB2, IIA, <sup>†</sup>		45	45	0	40	85
$\mathrm{IIB}^\dagger$		45	45	9-15	40	85
$\mathrm{III}^\dagger$		45-50	45-50	9-15	40	85-90
IIB, IIIB, IV	Poor pelvic anatomy, patient not readily treated with intracavitary insertions (barrel-shaped cervix not regressing, inability to locate					
	external os)	50	50	9-15	40	90
	Or interstitial	39.6-45	39.6-45	0–15	35-40* <sup>I</sup>	75 <b>-</b> 85*I

## **ABS recommendation for HDR**

- Keep total duration less than 8 weeks
  - Interdigitate HDR with EBRT
  - Started 2 weeks after EBRT weekly
  - If large tumor, start later twice weekly.
  - Keep HDR dose < 7.5 Gy

EBRT (Gy) @ 1.8 Gy/fraction	No. of HDR fractions	HDR dose/ fraction	EBRT (Gy) @ 1.8 Gy/fraction	No. of HDR fractions	HDR dose/ fraction
20	б	7.5	45	5	6.5
20	7	6.5	45	6	5.8
20	8	6.0	50.4	4	7.0
45	5	6.0	50.4	5	6.0
45	б	5.3	50.4	6	5.3
Ea	arly cervical Ca		Advanced	l Ca	

# **Results of Rx-cervix limited disease**

Authors		N° pts	Stage	5-yr survival	Local control
				(%)	(%)
Manchester 80-88	LDR	294	I/IIA	90-94 (DFS)	
Hunter 1993		45	IB	71 (OS)	
1993 (62	2)	70	IIB	52 (OS)	
Perez (87)	LDR	384	IB	85	90
		128	IIA	70	81
		353	IIB	72	77
Fletcher (35)	LDR	494	IB IIA MDAH	84	93
		207	IIB MDAH	70	82
French cooperative	group	229	I MDAH	89 (89)	93 (95)
LDR	· ·	315	IIA MDAH	81 (85)	83 (88)
Horiot (53)		314	IIB MDAH	76 (76)	80 (78)
Kim (66)	LDR	169	IB	82	89
		83	IIA	78	91
Lowrey (74	LDR	130	IB	81	88
2 .		64	IIA	74	84
Pernot (92)	LDR	173	IIA-B prox.	74	79
Coia (18)		203	IB	80	90
Joslin (64, 65)	HDR	95	1	94	97
		170	11	62	74
Petereit (93)	HDR	59	IB	86	85
		64	11	65	80
Vienna	HDR	42	IB/IIA	85 (DSS)	97
Pötter (96)		124	IIB	69 (DSS)	82

## **Cervix extended disease**

Authors	N° pts	Stage	5-yr survival (%)	5-y Local control (%)
Manchester 1993 LDR	50	111	34 OS	
Hunter 2001 (62)				
Perez (86)	293		52 DFS	59
LDR	20	IV	0	25
Houston MDAH (26,	73 a*	IB <sub>2</sub> IIB (bulk)	44 OS	67
28)	25 b*		60 OS	84
Fletcher LDR (73)	983	IIIB (UICC)	36 DSS	78
French cooperative	266	IIIA MDAH	61 OS (62)	68 (63)
group	216	IIIB MDAH	39 OS (50)	45 (57)
LDR (53)	32	IV	20 OS	18
Paris IGR (42)	58	Distal II	65 OS	78
LDR	416	IIIA-B, IV	42 OS	66
Pernot (92)	60	Distal IIB	70 OS	77
LDR	107	111	42 OS	54
Joslin (64, 65)	106	111	38 OS	56
HDR				
Petereit (93)	50	IIIB	33 OS	44
HDR				
Vienna	78	IIIB	48 DSS	65
	12		19 DSS	
HDR Pötter (96)	1 12	IVA	19033	48

# THANK YOU