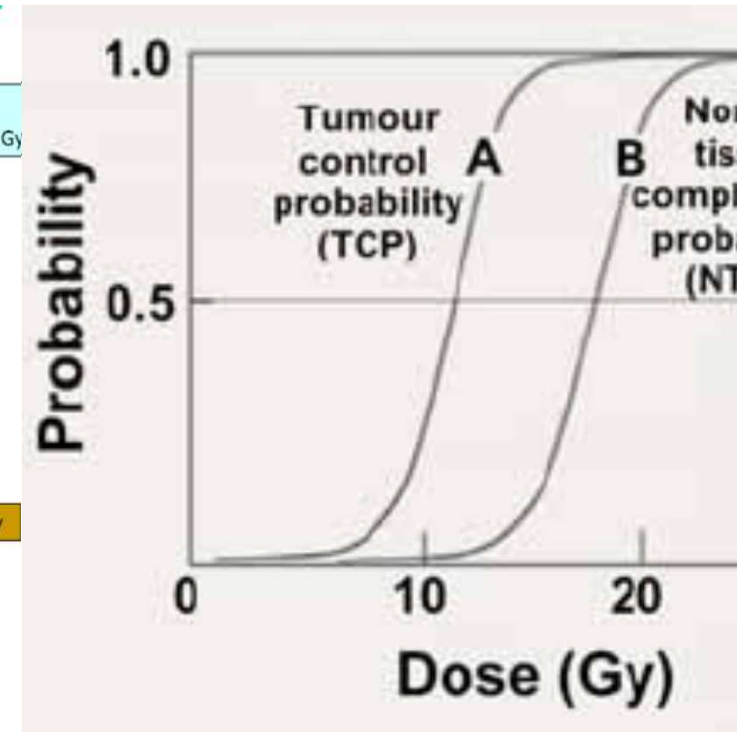
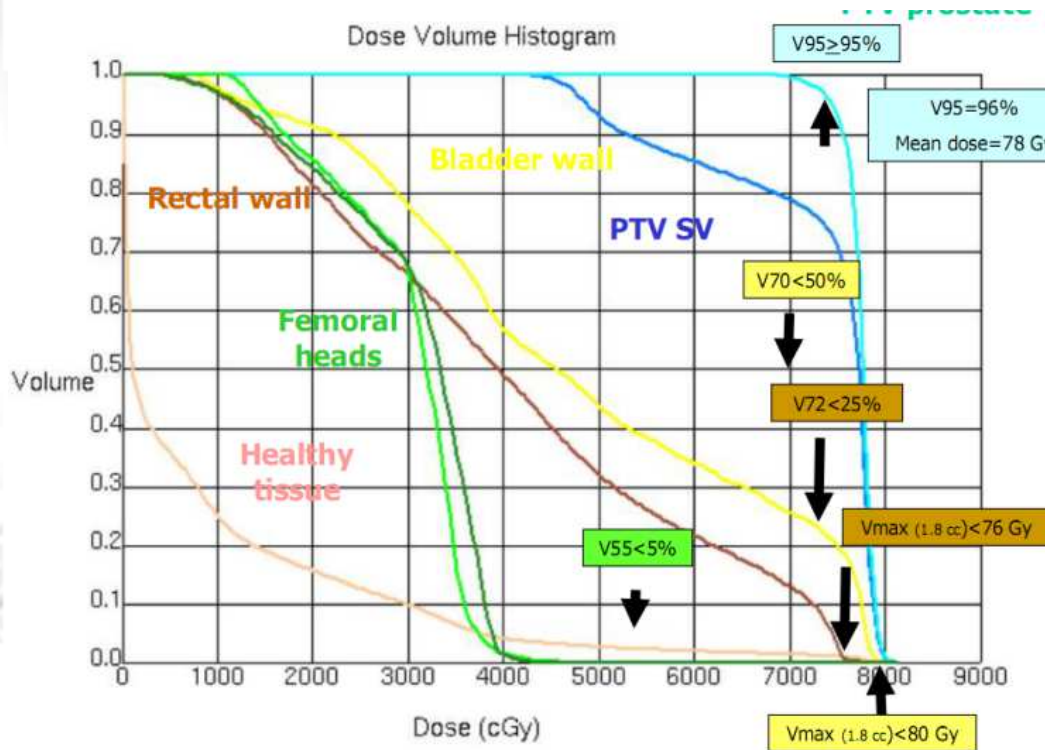
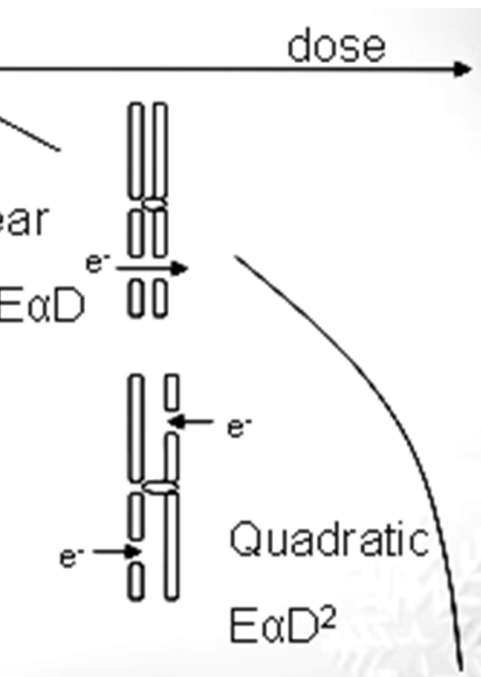


Mathematical Models in Radiotherapy



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S Rishikesh

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22nd December, 201

Road Map

- **Cell Survival Curve**
 - Multi Target Model
 - Linear Quadratic Model
 - Biological Effective Dose (BED)
 - Time Factor
- **Biological Model**
 - Tumor Control Probability (TCP)
 - Normal Tissue Complication Probability (NTCP)

• Clonogenic Cell:-

- A cell that is able to proliferate indefinitely and form a large colony from a single cell is said to be clonogenic.

• Cell Death

- **For proliferating cells: loss of capacity for sustained proliferation- that is loss of reproductive integrity.**
(2 Gy)

- **For differentiated cells: loss of a specific function.**
(100 Gy)

Example: for trigeminal neuralgia the dose required is

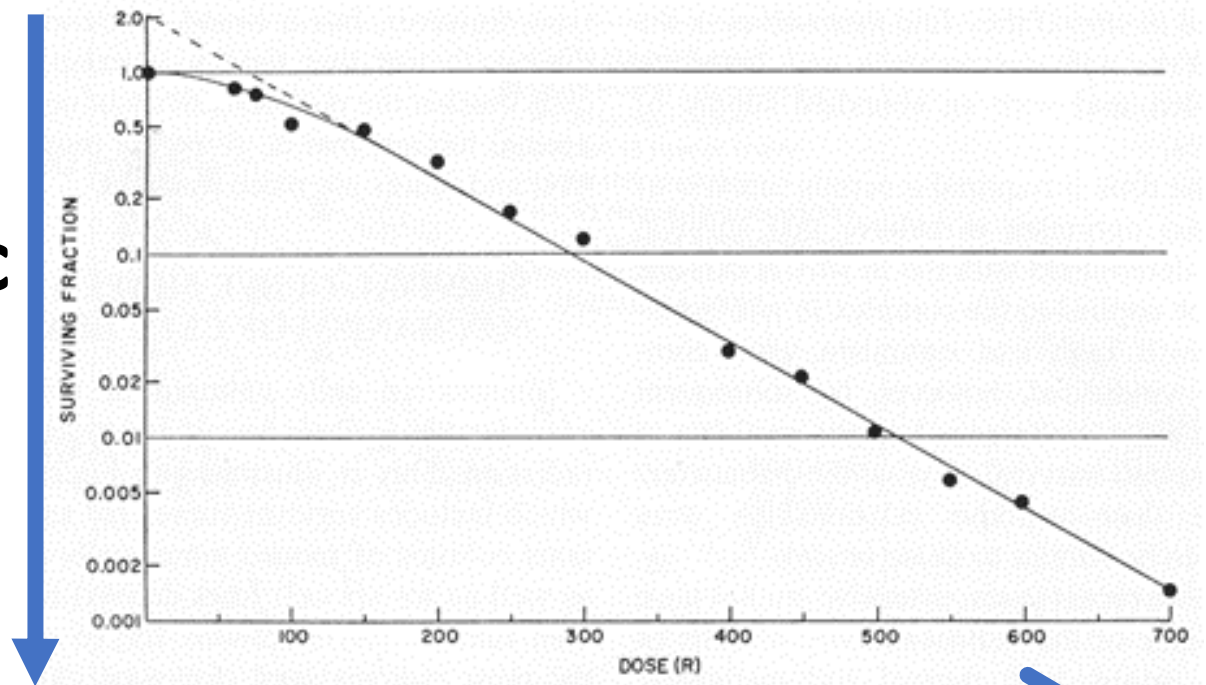
Cell Death

- **Following irradiation, cells may still be intact and able to produce proteins, synthesize new DNA and even go through few cell divisions**
- **However, if it has lost the capability to reproduce indefinitely, it is considered dead.**

What is a cell survival curve?

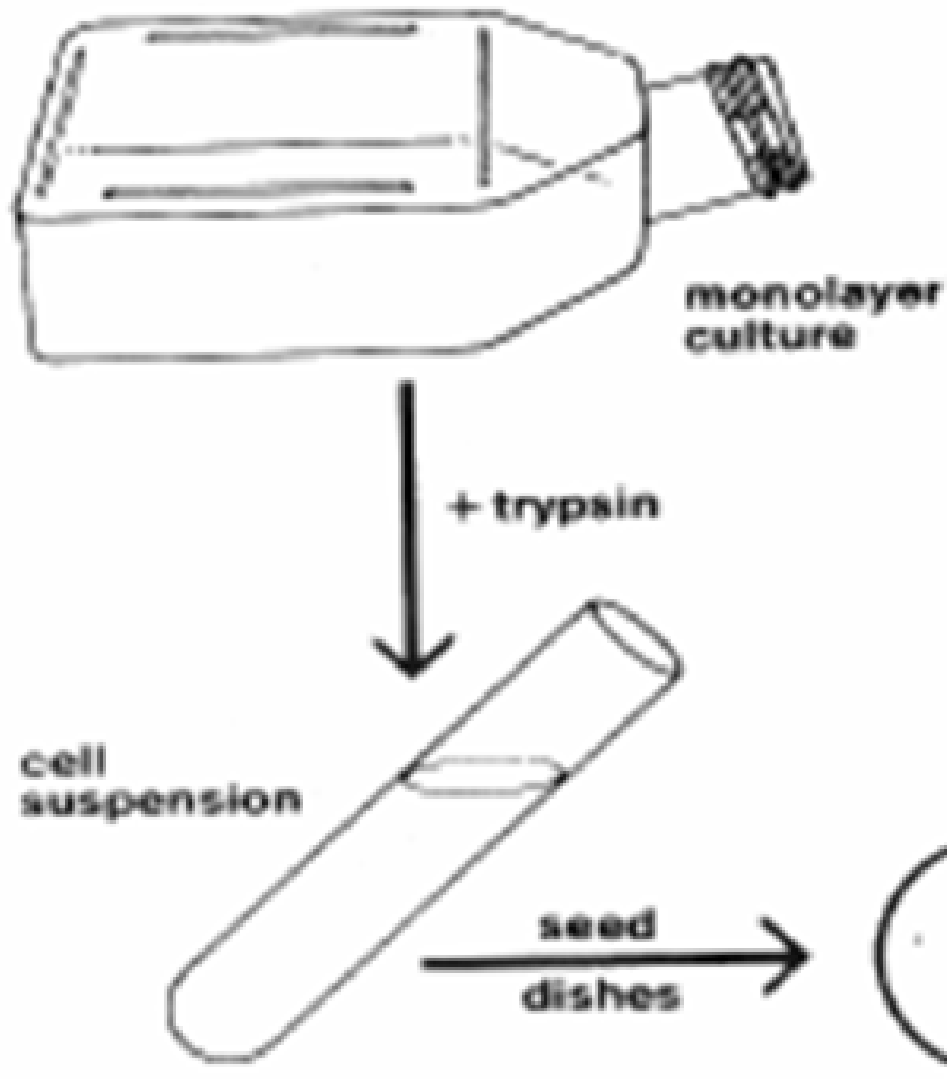
- A cell survival curve is a graphical representation of the fraction of cells surviving a given dose of radiation
- This graph is obtained by plotting the dose along **the linear x-axis** and the surviving fraction along the **logarithmic y-axis**

Logarithmic
Y-Axis



Linear X-Axis

In vitro cell culture



Take a specimen
from a tumour



Chop it into small
pieces



Prepare a single
cell suspension by
enzyme trypsin

OBSERVATION

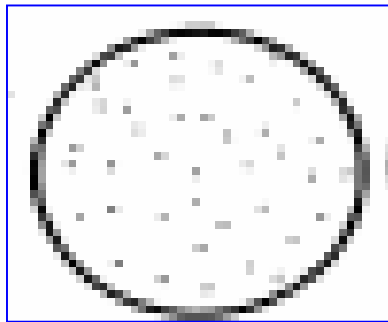
- **Some of the seeded single cells are still single and have not divided.**
- **Some cells die an apoptotic death.**
- **Some cells have managed to complete one or two divisions to form a tiny abortive colony.**
- **Many of the cells have grown into large colonies that differ little . These cells are said to have survived, because they have retained their reproductive integrity.**

Plating efficiency= What is the efficiency of the Petri dish to form colonies from known number of seeded cells

Plating Efficiency

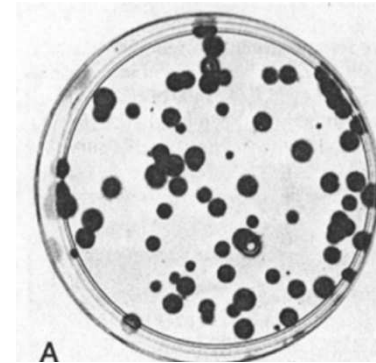
Definition :- Percentage of cells seeded that grow into colonies is known as **plating efficiency**.

**Plating efficiency = no of colonies counted X 100
cells seeded**



100 cells

Incubate for 1-2 week



90 Colonies

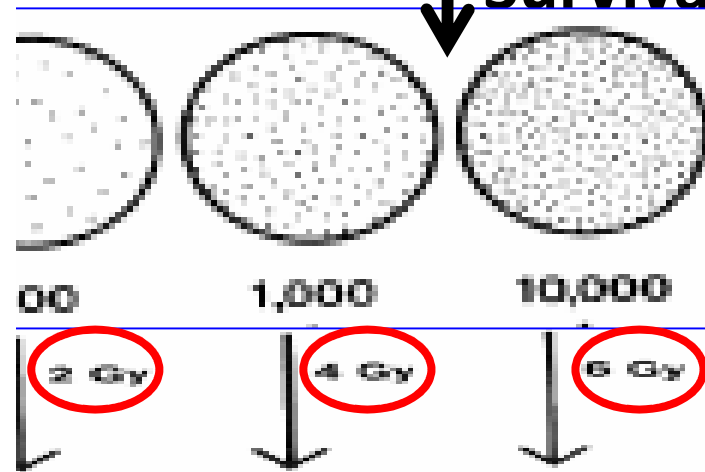
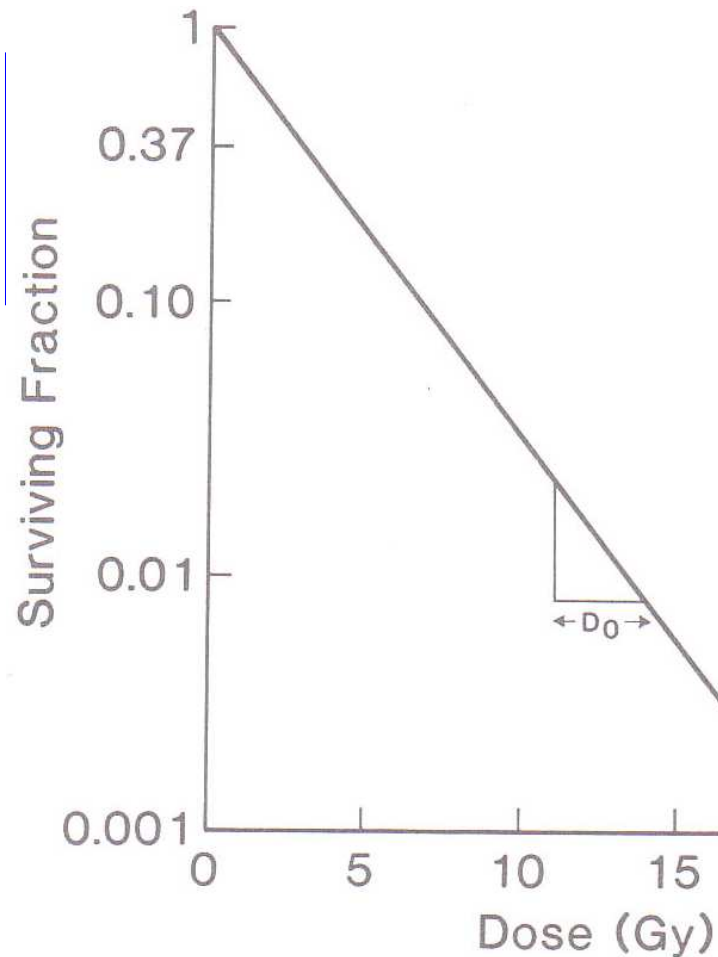
$$PE = \frac{90 \times 100}{100} = 90\%$$

Surviving fraction =
Colonies counted

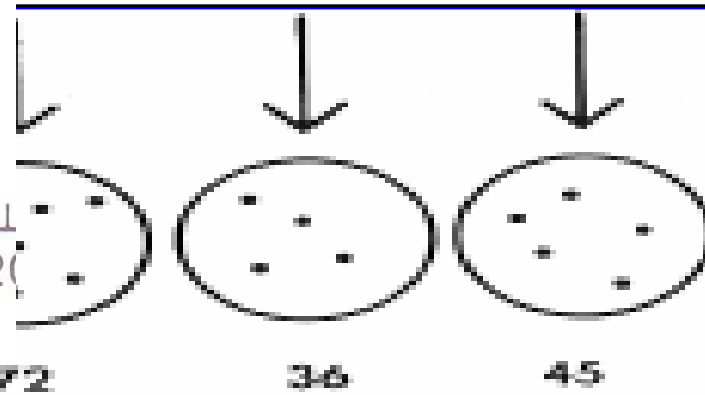
Cells seeded x (PE/100)

Cell Survival Curve

↑ Dose of Radiation
↓ Survival Fraction



1-2 weeks



A

90 Colonies

Plating Efficiency = 90%

Surviving fraction =

$$\frac{72}{400 \times 0.9}$$

0.2

$$\frac{36}{1000 \times 0.9}$$

0.04

$$\frac{45}{10,000 \times 0.9}$$

0.005

Cell Survival Curve of Micro-organism

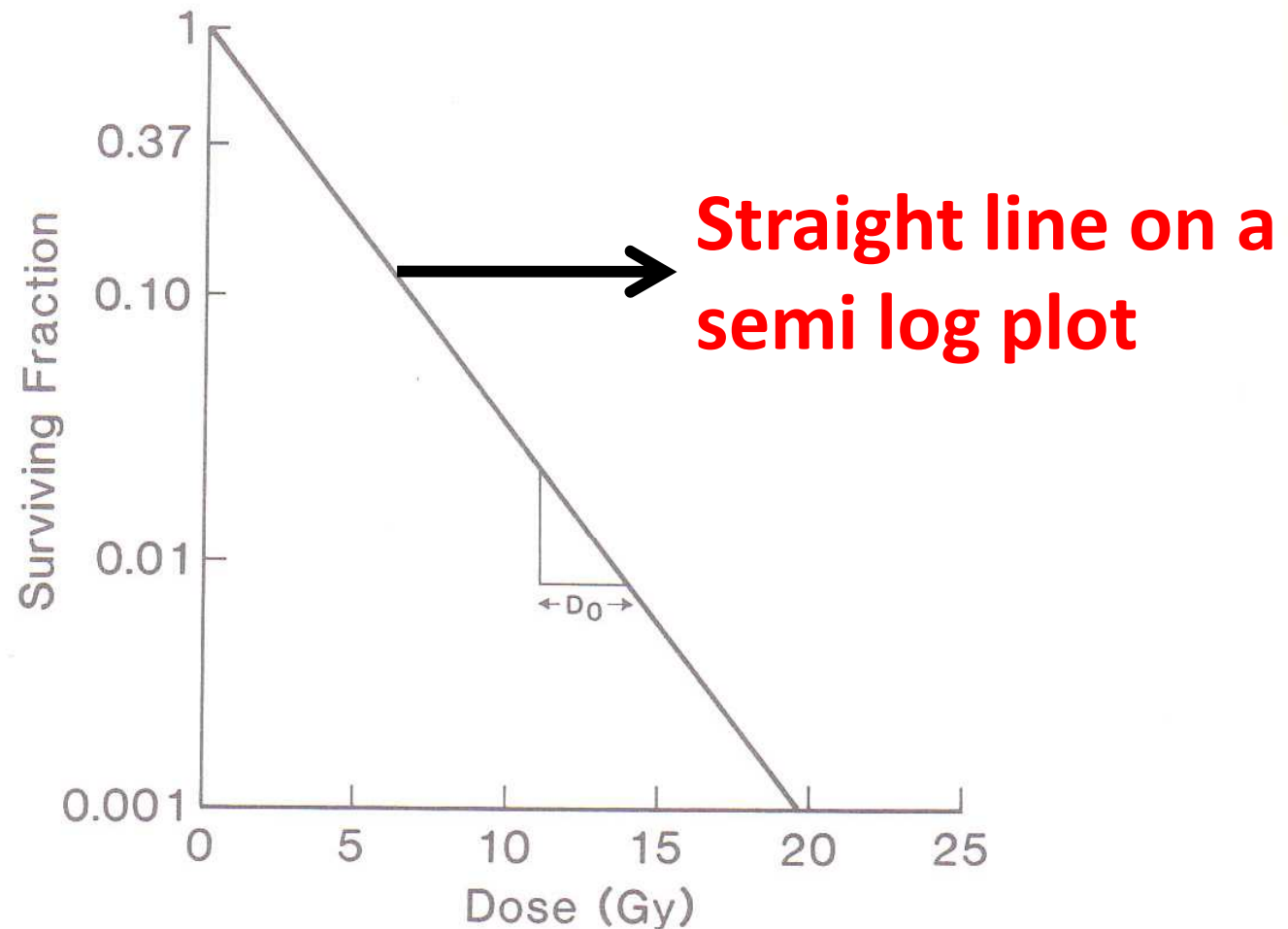
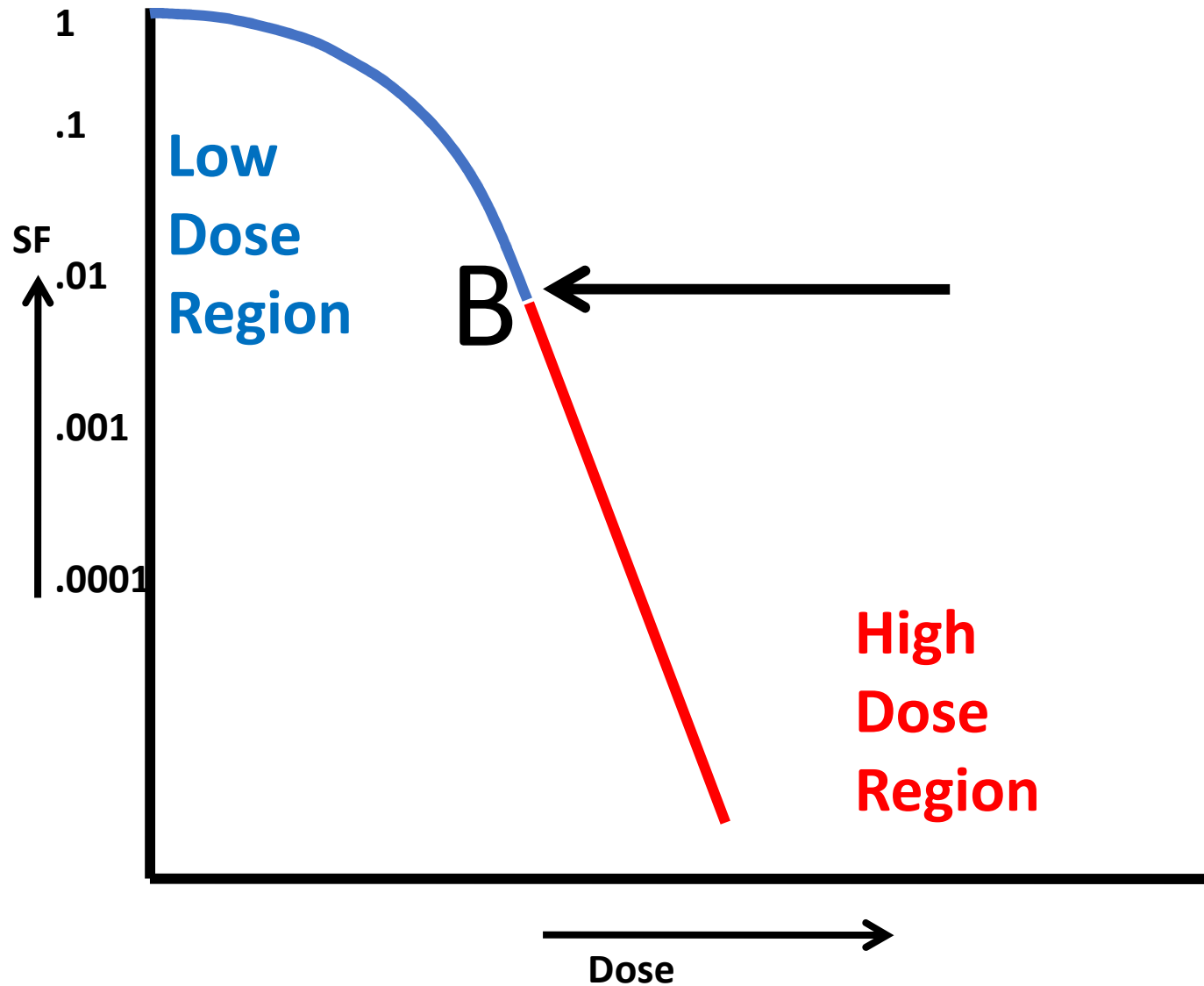


FIG 3-4.

Survival curve for bacteria (*Escherichia coli*), showing that in this system survival is a simple exponential function of dose.

Mammalian Cell Survival Curve



➤ Initial portion is continuously bending at low dose region till it reaches at point B.

➤ At higher dose region the curve becomes a straight line.

Two Models to describe mammalian cell survival curve

- **Multi Target Model**
- **Linear Quadratic (LQ) Model**

Multi Target Model

- Each cell contain more than one target (may be assumed n number of target and n may be any number more than one)
- In order to bring cell death by radiation, all the target should be deactivated.
- If $n-1$ targets are hit then cell survives.
- There are two type of cell killing taking place simultaneously to inactivate n target resulting into cell death.

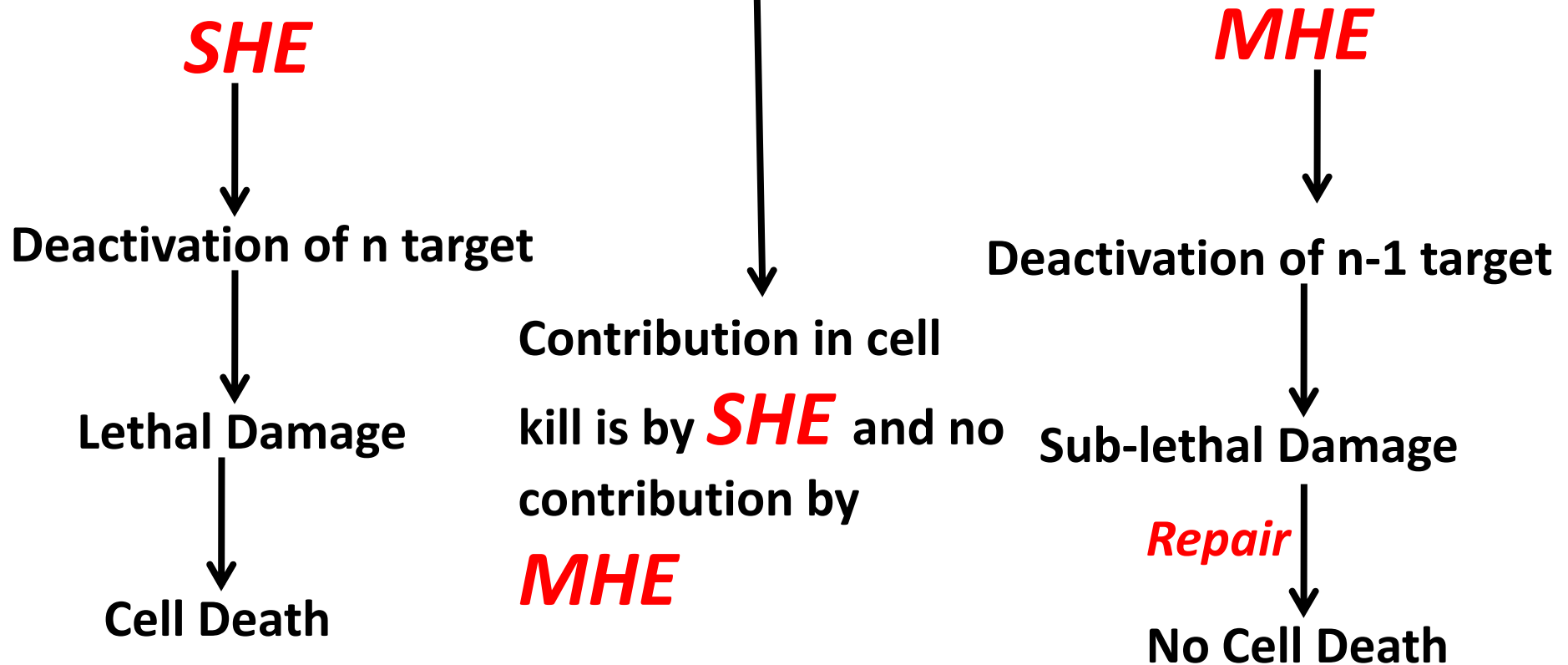
Low Dose Region

- *Cell kill by single hit event (SHE)*

High Dose Region

- *Cell kill by multiple hit event (MHE)*

Low Dose Region

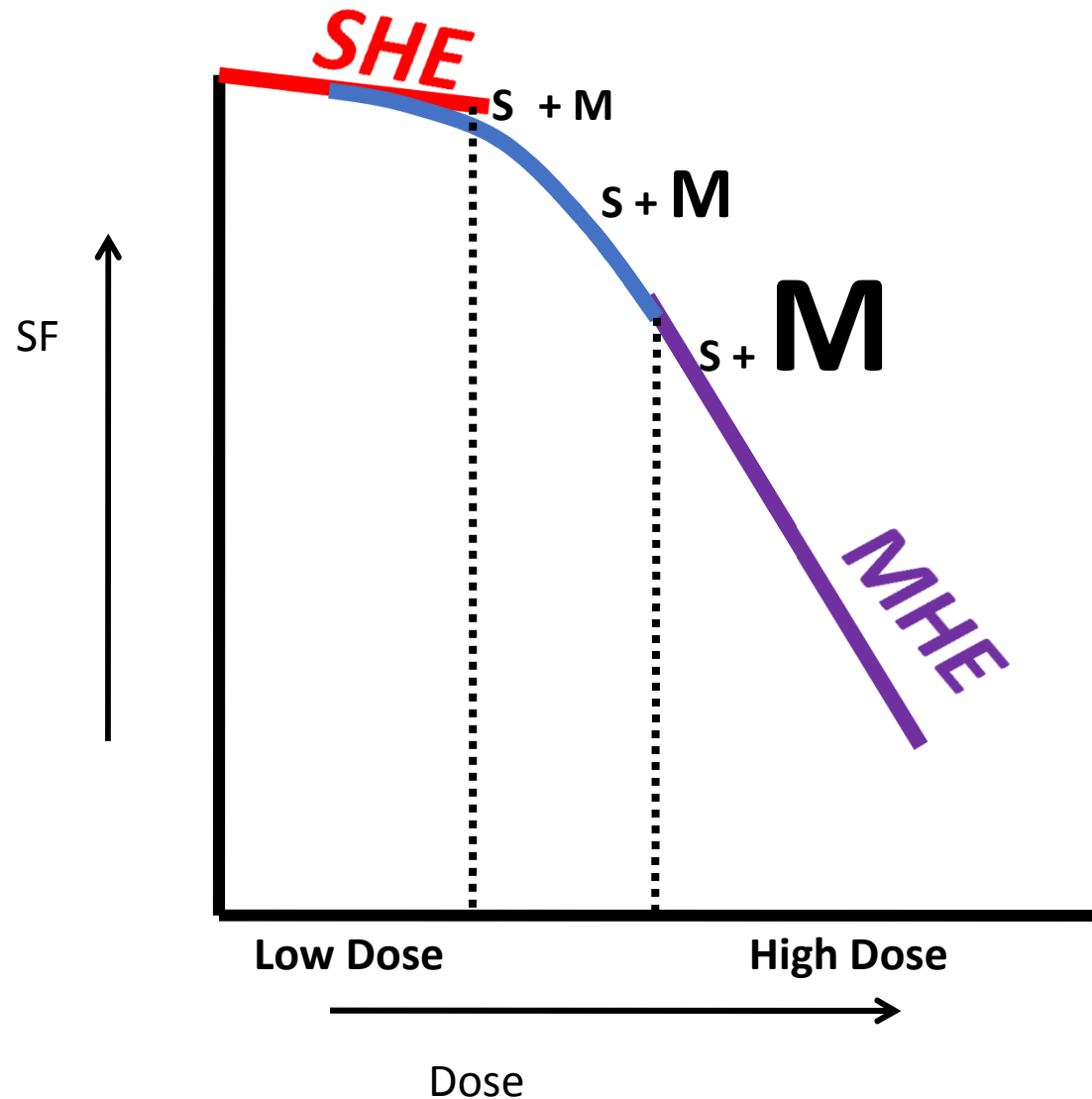


High Dose Region

Main contribution in cell kill is by **MHE**.

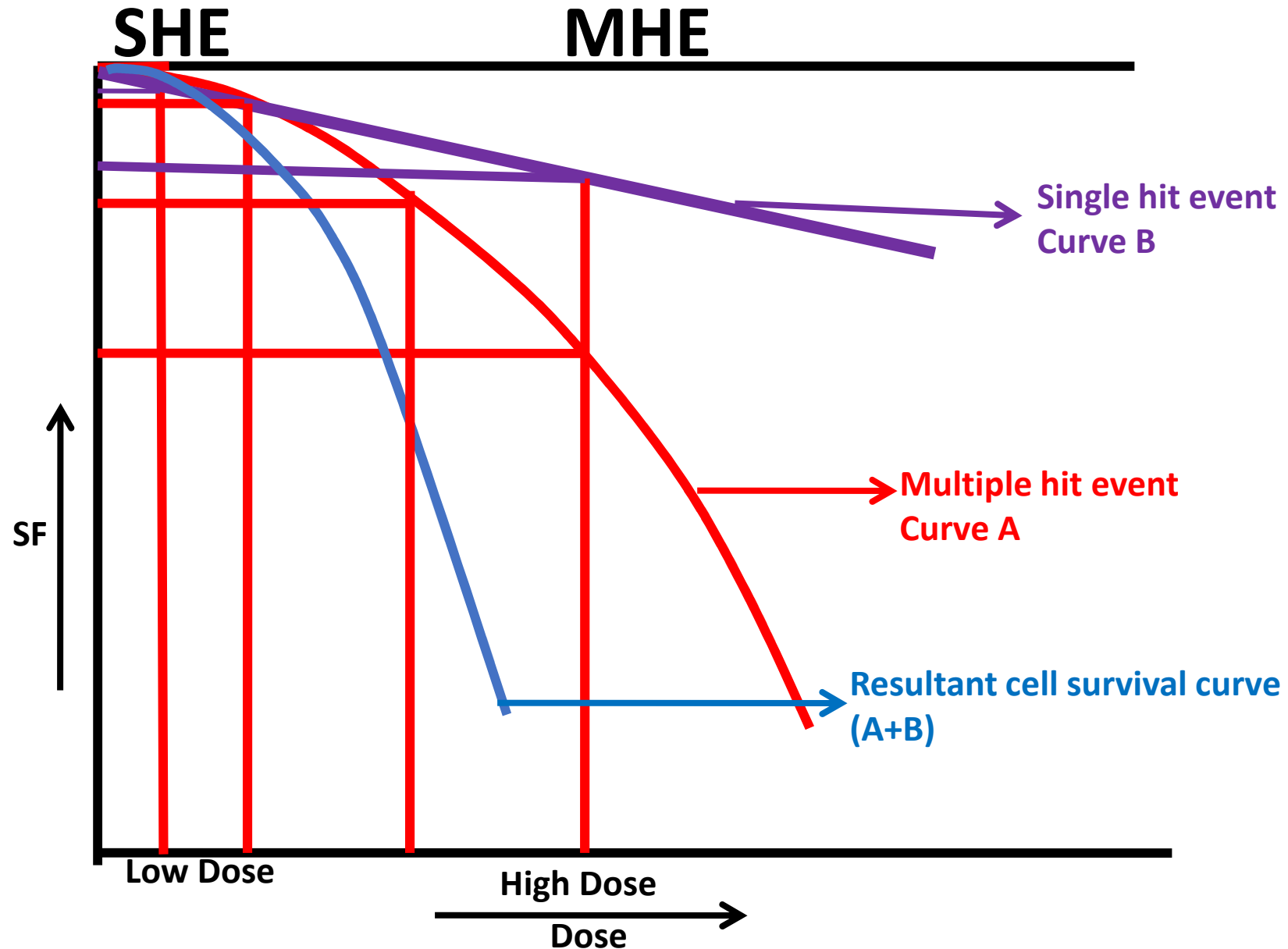
Relative contribution by **SHE** is small.

Multi Target Model



As dose increases the probability of deactivation of n target by **MHE** also increases and **MHE** also start contributing in total cell kill.

Multi Target Model



Multi Target Model

- **This is a theoretical model as we know there is no threshold dose of radiation below which, there is no damage.**
- **While this model based on quasi threshold dose.**
- **This model can not be used in clinical practice.**
- **Fails to identify that acute and late reacting tissue behave differently with radiation.**

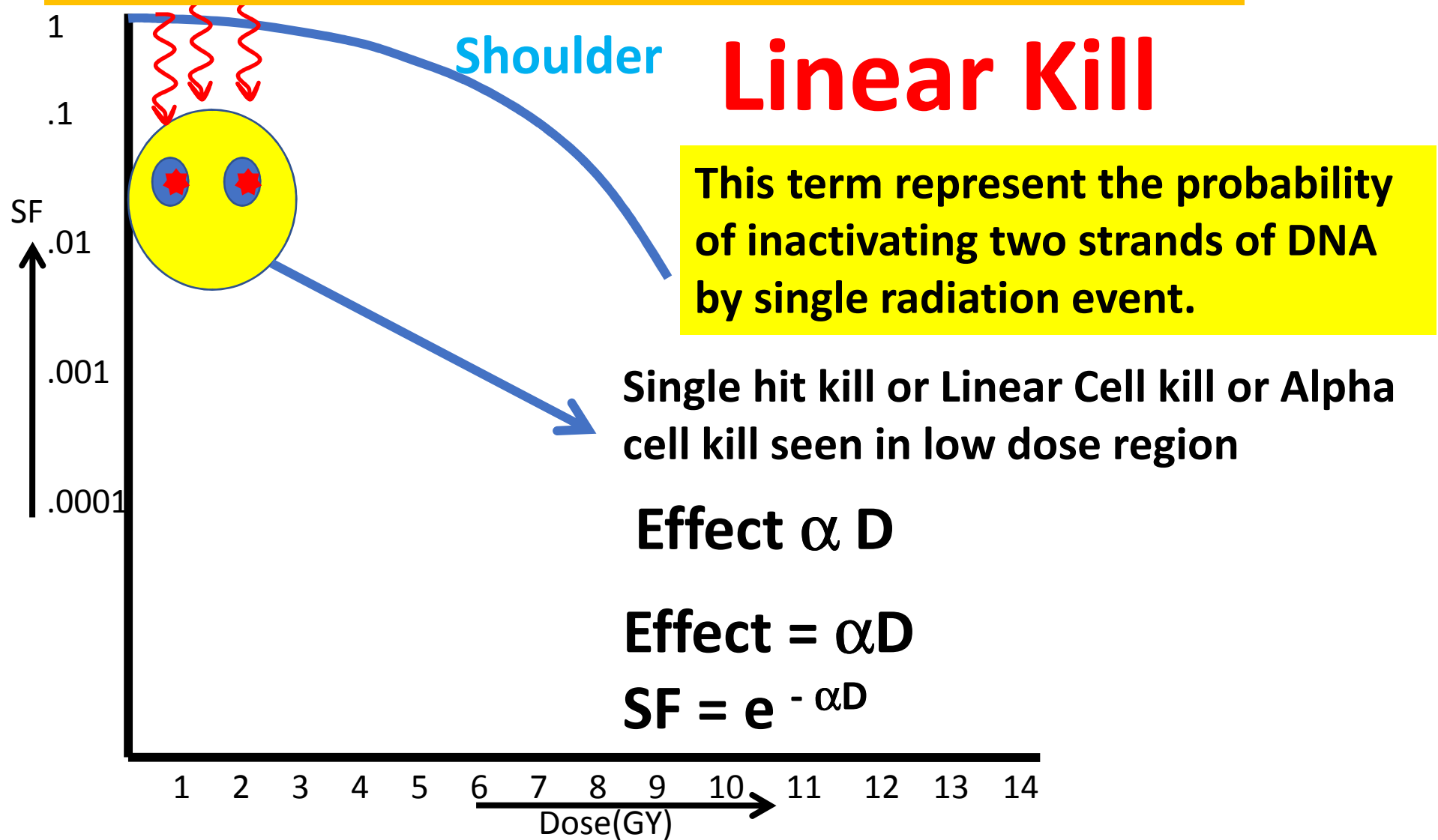
Two Models to describe mammalian cell survival curve

- **Multi Target Model**
- **Linear Quadratic (LQ) Model**

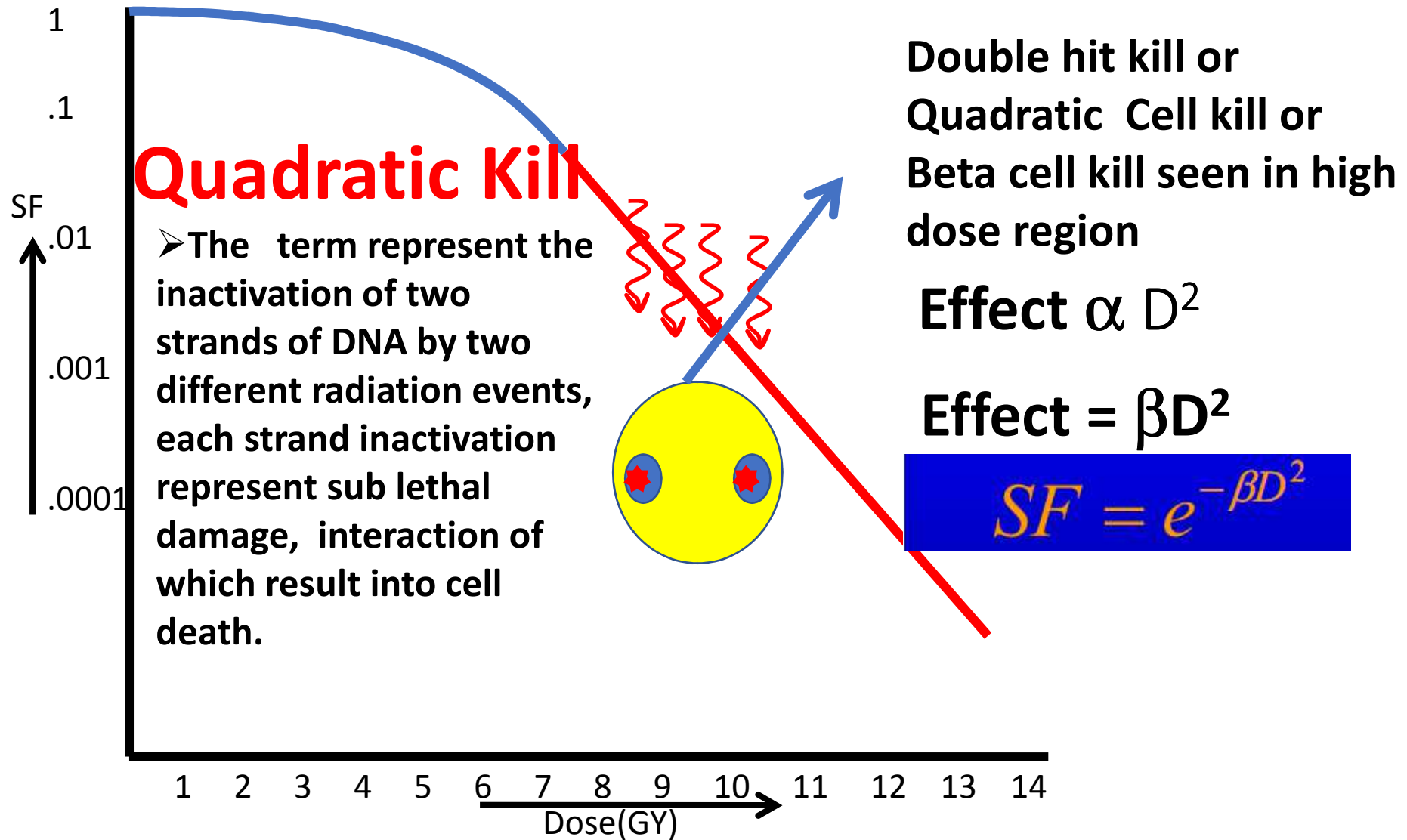
➤ Only one target has to be inactivated.

➤ This target is considered to be two strands of DNA

Linear Quadratic model (LQ Model)

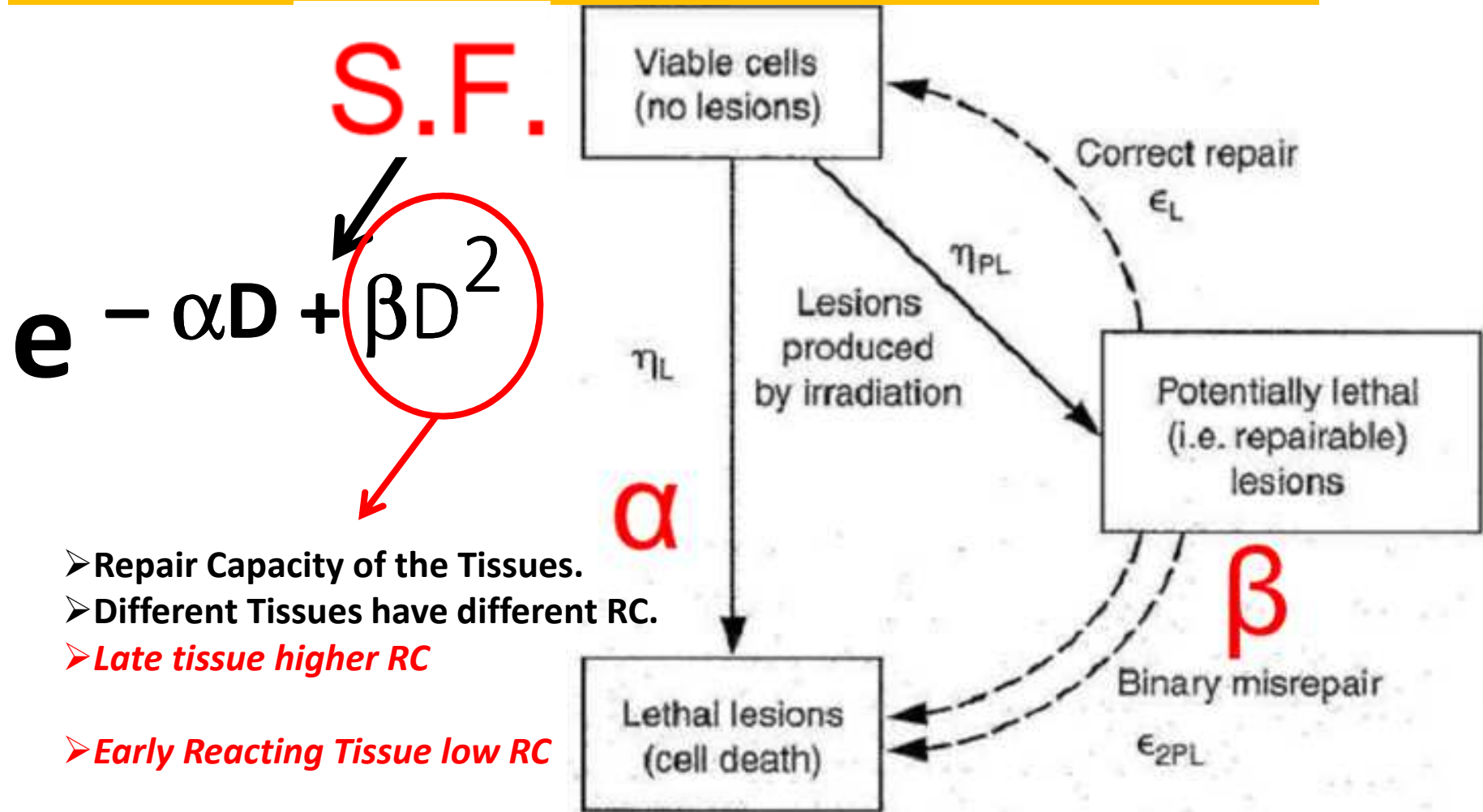


Linear Quadratic model (LQ Model)



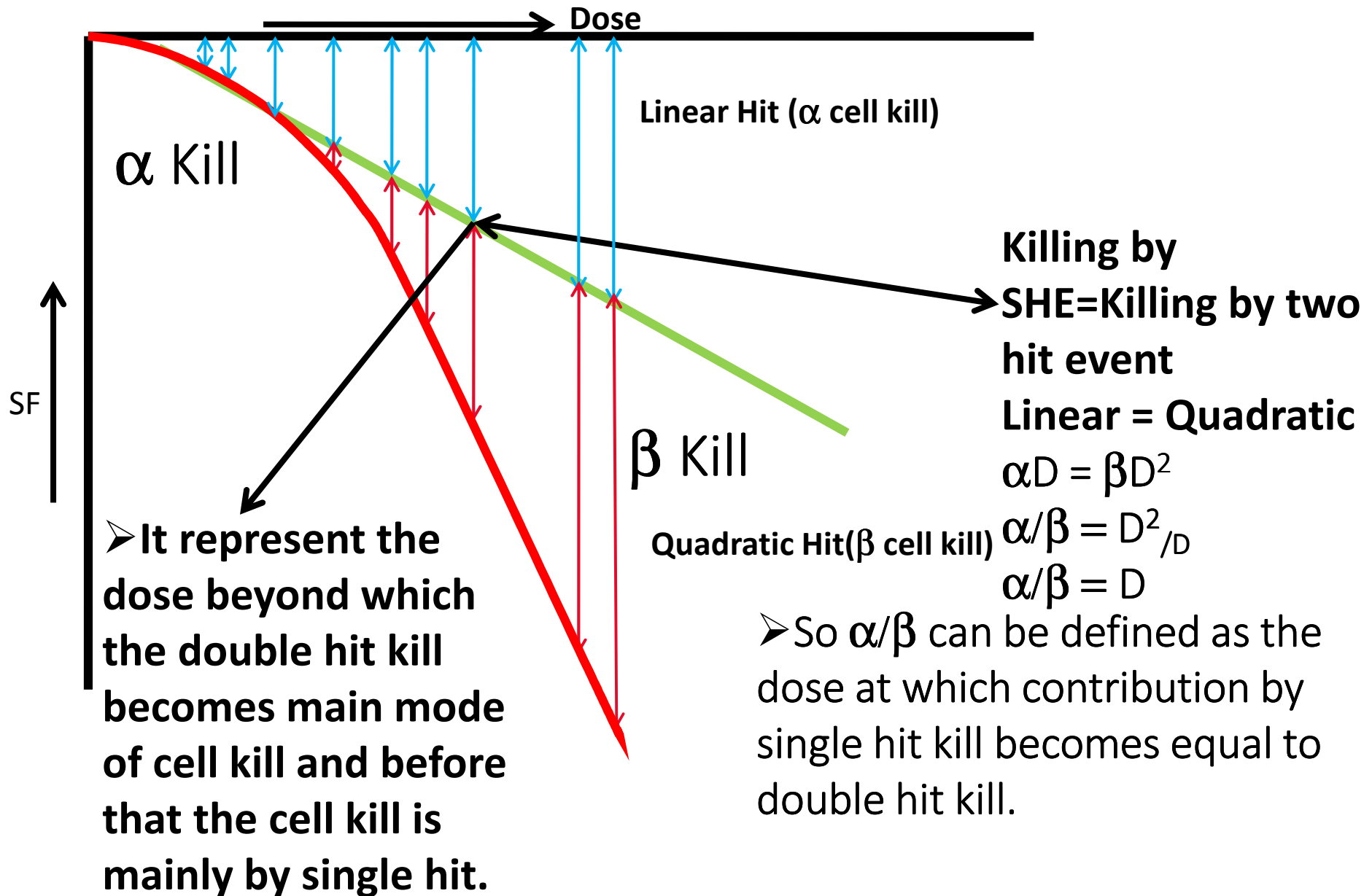
Double hit kill is similar to the MHE

Linear Quadratic model (LQ Model)



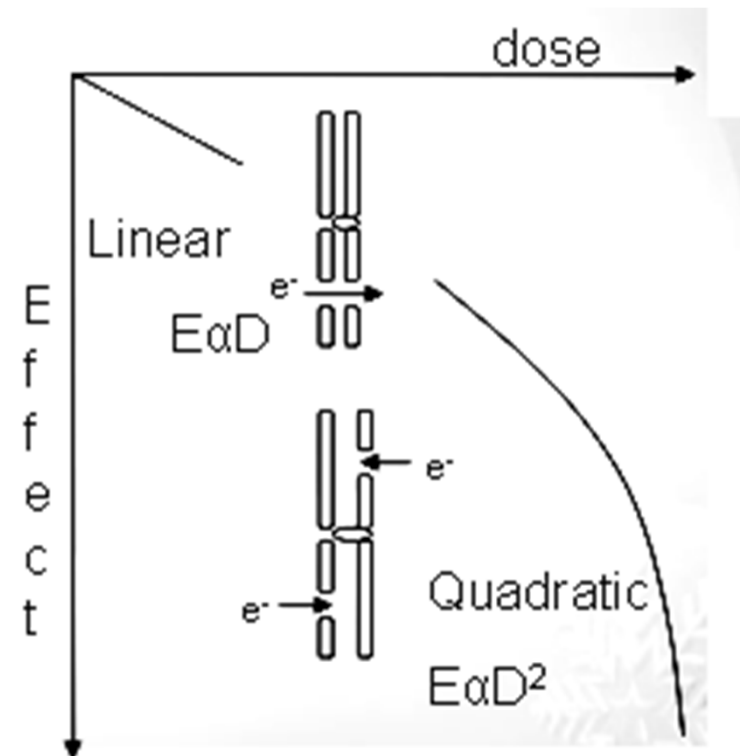
The sum of the two process of cell killing (linear and quadratic) will decide the final survival fraction.

Linear Quadratic model (LQ Model)



WHAT IS α/β ?

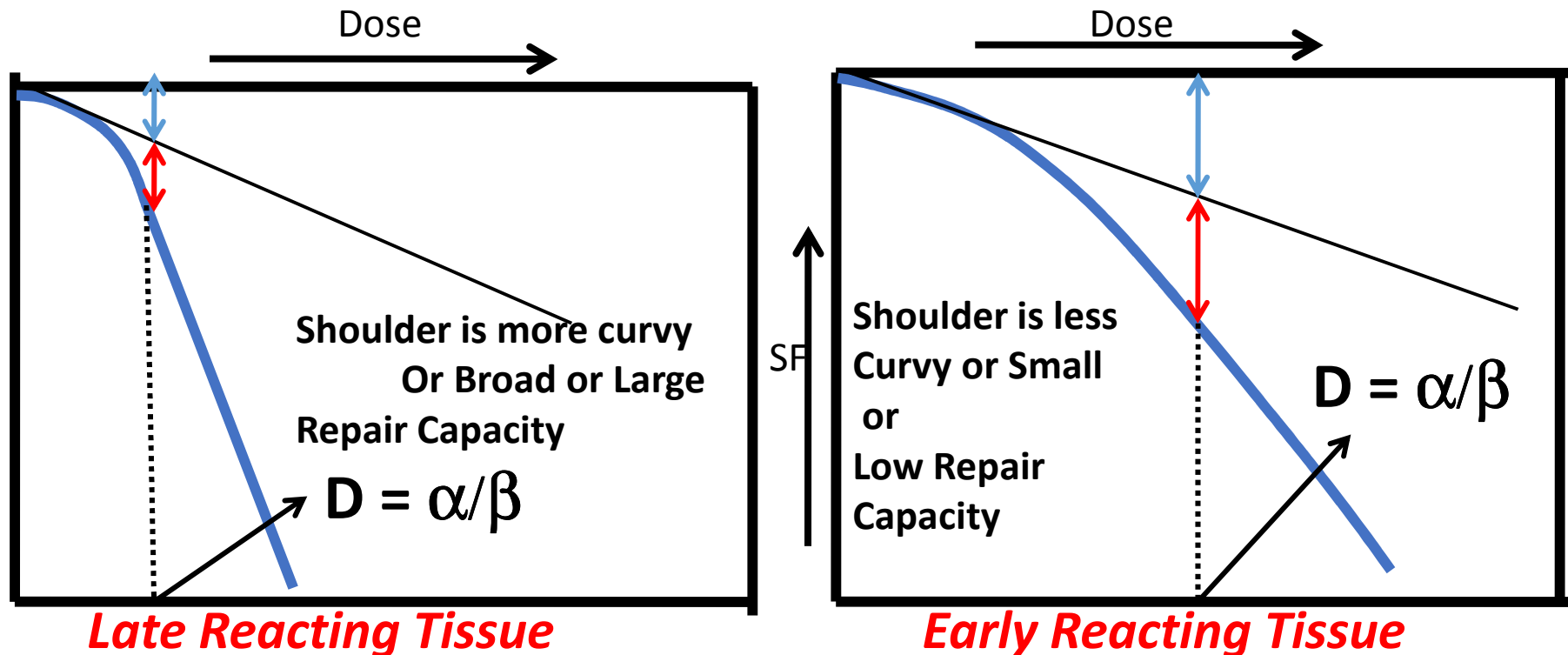
- $\alpha/\beta = D$, dose at which the contribution in cell kill by both processes becomes equal.
- α/β also represents the point beyond which the curve becomes a straight line and predominantly double hit events take place.



α/β Ratio defines “curviness” of survival curve

Based on α/β ratio, the body tissues have been divided into two category.

Malignant Tumor behave like Early Reacting Tissue and have similar shape of cell survival curve and same α/β Ratio i.e. an average of 10



$\alpha/\beta = 1\text{Gy to } 7\text{ Gy (3Gy)}$
Responsible for late effect of radiation
Eg. Spinal cord, urinary bladder, kidney, liver etc.

$\alpha/\beta = 6\text{Gy to } 15\text{ Gy (10Gy)}$
Responsible for acute effect of radiation
Eg, skin, mucosa, lining of intestine, bone marrow etc.

Calculated α/β ratios for some tissues

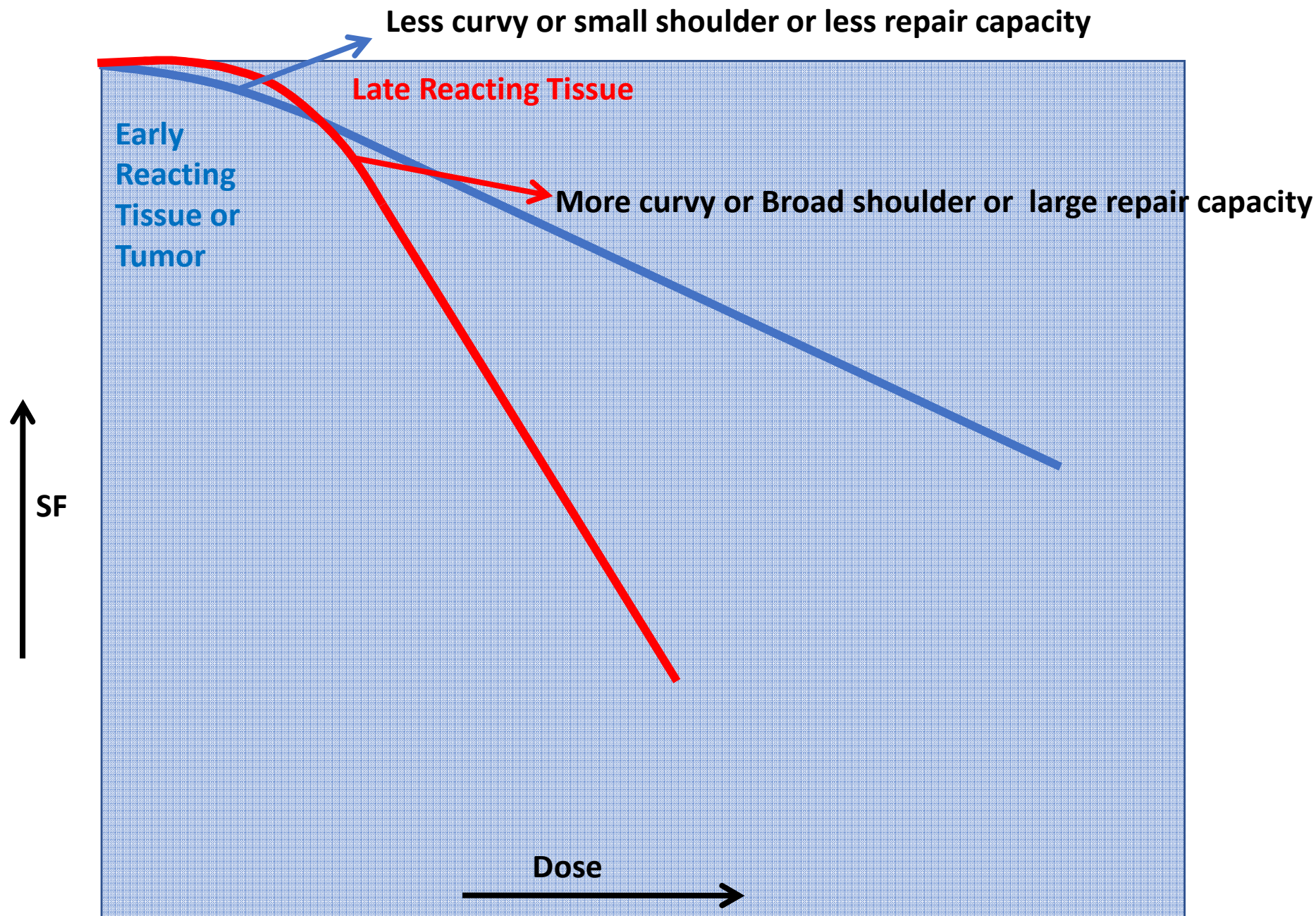
TABLE 22.1. *Ratio of Linear to Quadratic Terms From Multifraction Experiments*

Reactions		α/β , Gy
Early		
Skin	Average 10	9–12
Jejunum		6–10
Colon		10–11
Testis		12–13
Callus		9–10
Late		
Spinal cord	Average 3	1.7–4.9
Kidney		1.0–2.4
Lung		2.0–6.3
Bladder		3.1–7

Calculated α/β ratios for some tumors

Tumors	
Head and neck: nasopharynx	16 (-11; 43) Gy
Vocal cord	~13 Gy
Buccal mucosa	~6.6 (2.9; ∞) Gy
Tonsil	7.2 (3.6; ∞) Gy
Larynx	14.5 (4.9; 24) Gy
Lung: squamous cell carcinoma	~50-90 Gy
Cervix: squamous cell carcinoma	>13.9 Gy
Skin	
Squamous cell carcinoma	8.5 (4.5; 11.3) Gy
Melanoma	0.6 (-1.1; 2.5) Gy
Prostate	1.1 (-3.3; 5.6) Gy
Breast (early-stage invasive ductal, lobular, and mixed)	4.6 (1.1; 8.1) Gy
Esophagus	4.9 (1.5; 17) Gy
Liposarcoma	0.4 (-1.4; 5.4) Gy

Average 10



Cell Survival Curve of Early and Late Reacting Tissues

Biological Effective Dose(BED)

For a single acute dose D, the biologic effect is given by

$$E = \alpha D + \beta D^2 \quad (1)$$

For n well separated fractions of dose d, the biologic effect is given by

$$E = n(\alpha d + \beta d^2) \quad (2)$$

As suggested by Barendsen, this equation may be rewritten as

$$E = (nd)(\alpha + \beta d)$$

$$\begin{aligned} E &= (nd)(\alpha + \beta d) \\ &= (\alpha)(nd) \left(1 + \frac{d}{\alpha/\beta} \right) \end{aligned} \quad (3)$$

$$= (nd) \times \left(1 + \frac{d}{\alpha/\beta} \right) \quad (4)$$

$$\frac{E}{\alpha} =$$

Biologically Effective Dose (BED) =

Biological Effective Dose(BED)

$$(BED) = \frac{E}{\alpha} = (\text{total dose}) \times (\text{relative effectiveness})$$

$$(\text{relative effectiveness}) = \left(1 + \frac{d}{\alpha/\beta}\right) \quad \text{Same} \quad RE \propto \frac{1}{\alpha/\beta}$$

- Late Reacting tissue α/β ratio is low so RE is more
- Early Reacting tissue α/β ratio is high so RE is less
- So increasing the dose per fraction will have more effect on late reacting tissues. Eg

If dose/fx = 3 Gy

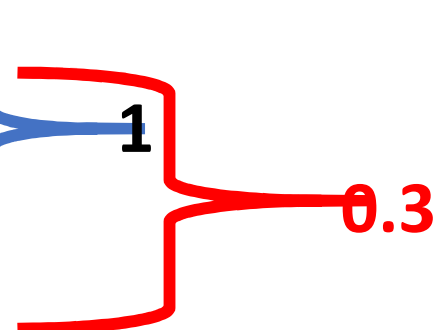
$$RE(3Gy) = 1 + 3/3 = 2 \text{ for late reacting tissue}$$

$$RE(3Gy) = 1 + 3/10 = 1.3 \text{ for early reacting tissue}$$

dose/fx is doubled i.e. 6 Gy

$$RE(6Gy) = 1 + 6/3 = 3 \text{ for late reacting tissue}$$

$$RE(6Gy) = 1 + 6/10 = 1.6 \text{ for early reacting tissue}$$



Iso-effective total dose

$$\frac{E}{\alpha} = (\text{total dose}) \times (\text{relative effectiveness})$$

$$(BED) = \frac{(nd)}{(D)} \times \left(1 + \frac{d}{\alpha/\beta}\right) \quad (4)$$

Conventionally we give 60 Gy in 30f with 2 Gy per f.

If dose per f is increased from 2 to 4 Gy the isoeffective total dose will be

$$(BED)_2 = (BED)_1$$

$$D_2 \times \left(1 + \frac{d_2}{\alpha/\beta}\right) = D_1 \times \left(1 + \frac{d_1}{\alpha/\beta}\right)$$

FOR LATE REACTING TISSUES

$$D_2 \times (1 + 4/3) = 60 \times (1 + 2/3)$$

$$D_2 = 60 \times 5/3 \times 3/7 = 43 \text{ Gy}$$

FOR EARLY REACTING TISSUES

$$D_2 \times (1 + 4/10) = 60 \times (1 + 2/10)$$

$$D_2 = 60 \times 12/10 \times 10/14 = 52 \text{ Gy}$$

**Always calculate
Iso-effective dose
based on α/β ratio
of late reacting
tissue**

Time Factor in L-Q Model

- **The effect of accelerated repopulation will depends upon**
 - **Timing of repopulation during radiation treatment.**
 - **Potential tumor doubling time.**
 - **Total duration of repopulation.**

Overall Treatment Time ← Time when Repopulation Start

So Accelerated repopulation = $\frac{0.693}{0.3/\text{Gy}} \times \frac{T - T_k}{T_{\text{pot}}}$

21 to 28 days after beginning of radiotherapy in Head & Neck cancer.

2 to 25 days with a median of 5 days

6 weeks (39 days) schedule

Dose equivalent to accelerated repopulation = $\frac{0.693}{0.3} \times \frac{(39 - 21)}{5}$

7 weeks (46 days) schedule

Dose equivalent to accelerated repopulation = $\frac{0.693}{0.3} \times \frac{(46 - 21)}{5} = 11.6 \text{ Gy}_{10}$

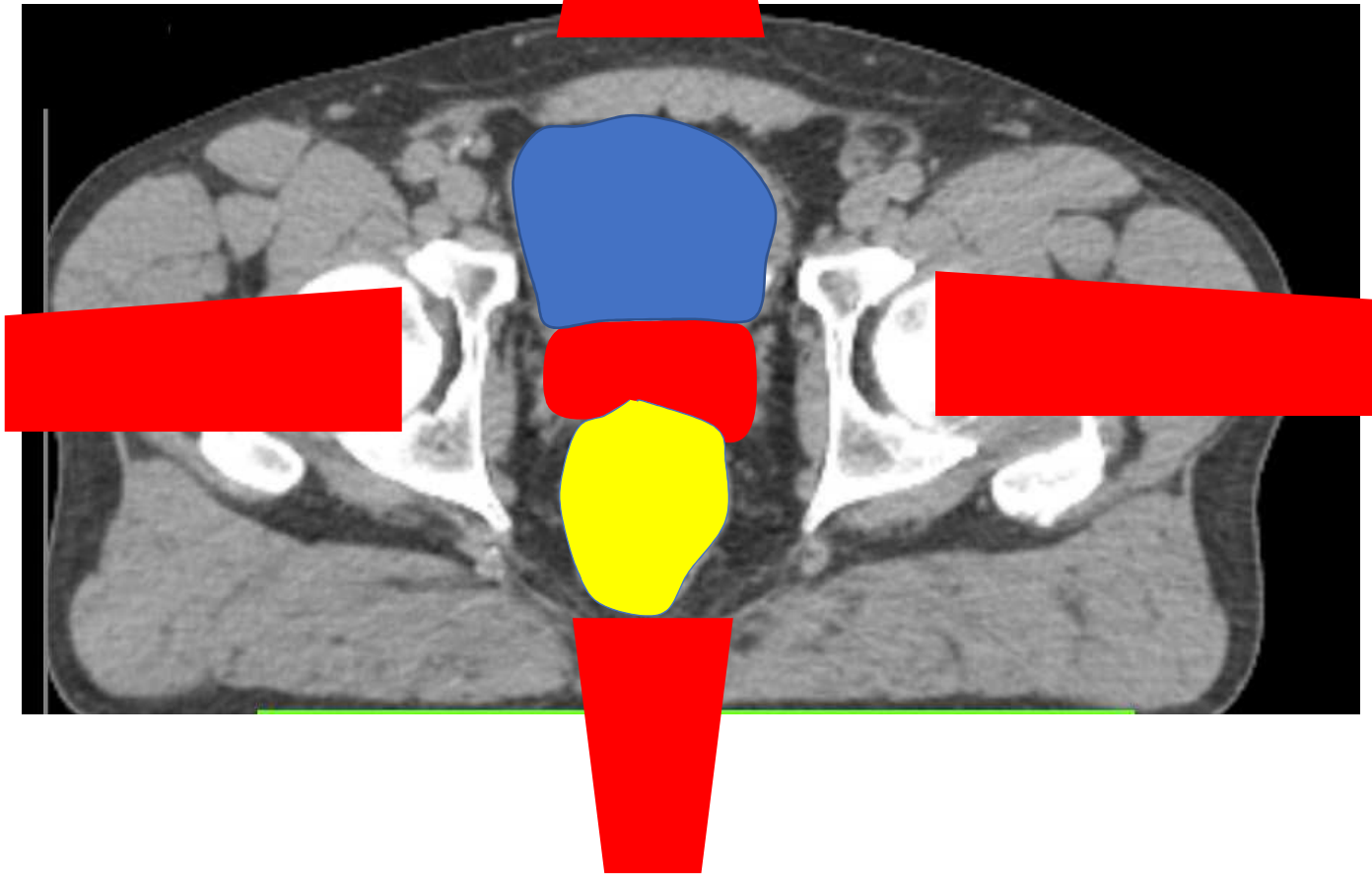
0.46Gy per day

Dose of radiation which goes waste

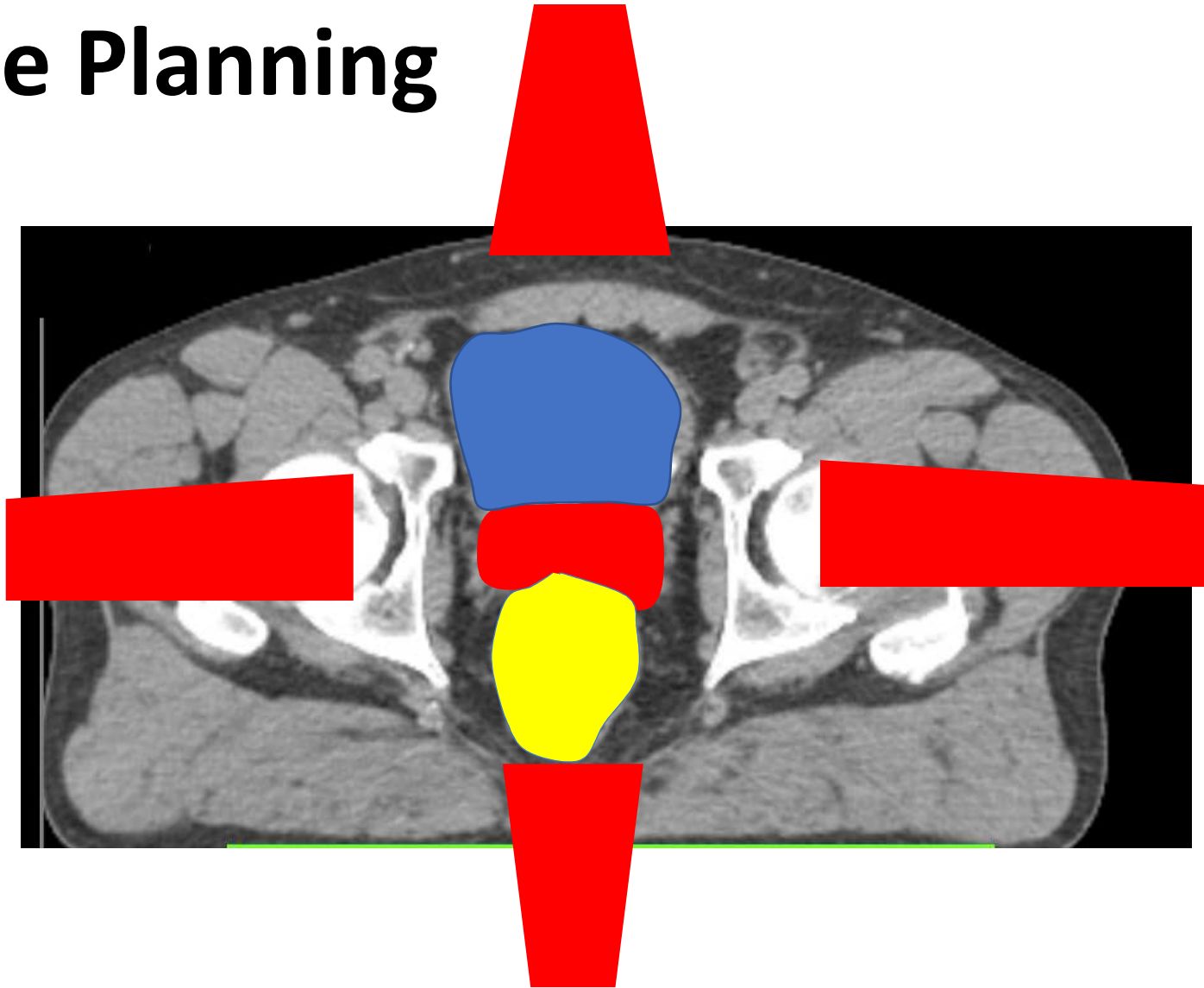
So this much of dose is to be reduced from BED on account of repopulation. This also shows as overall treatment time increases the BED decreases.

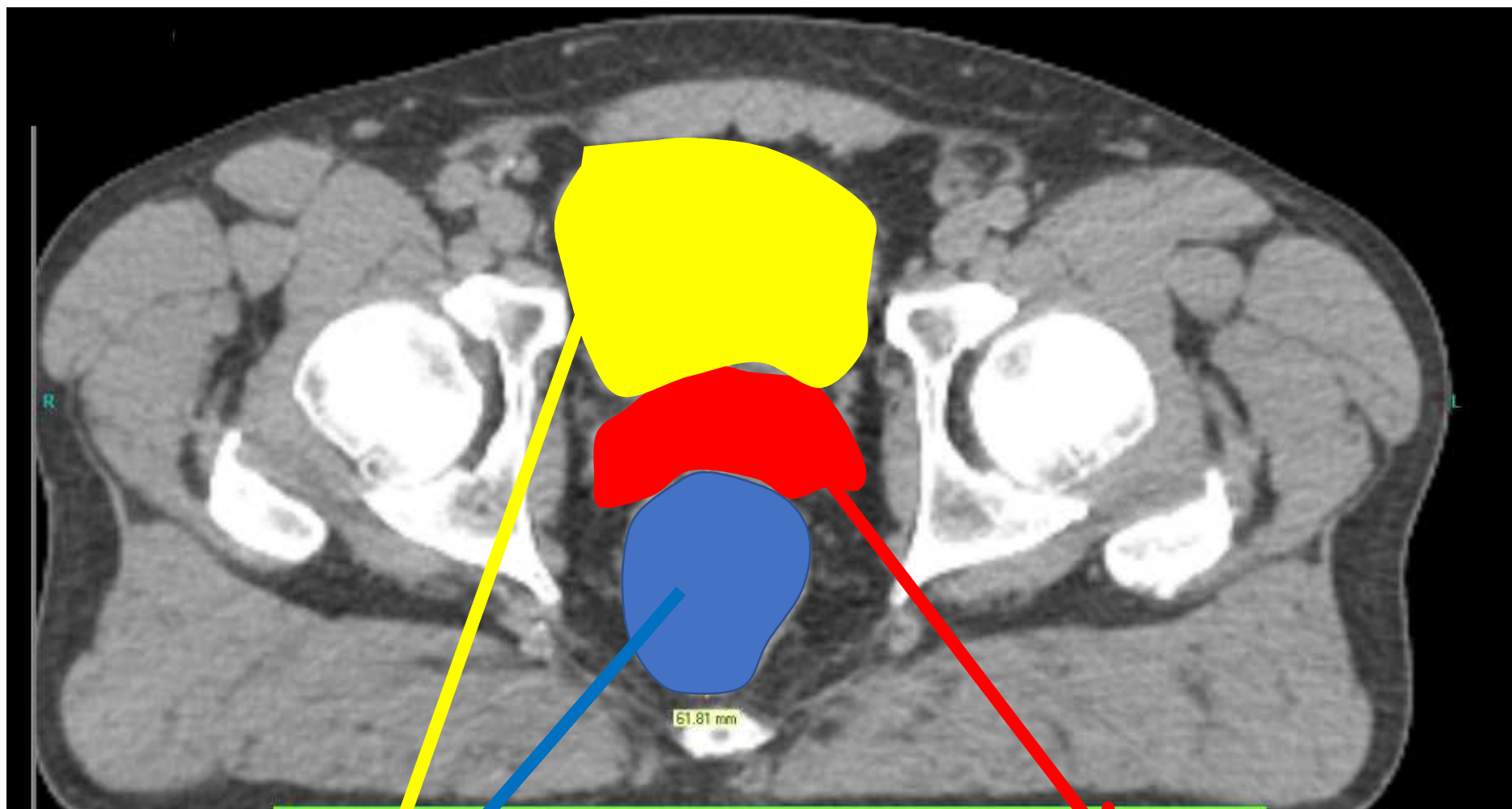
Biological Model

Forward Planning



Inverse Planning





Normal Tissue Complication



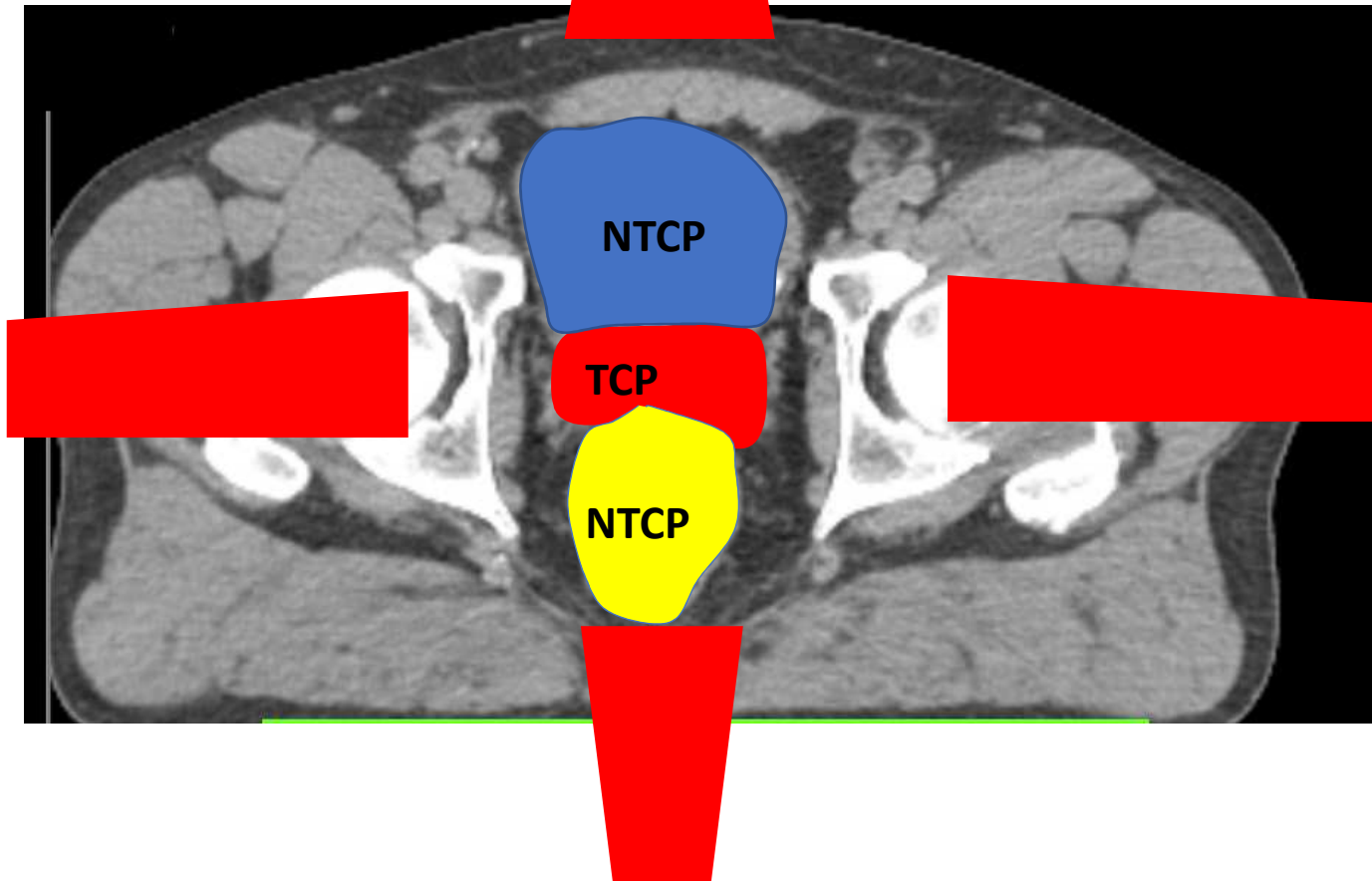
Normal Tissue Complication Probability(NTCP)

Tumor Control



Tumor Control Probability (TCP)

Biological Based Planning



Therapeutic Ratio

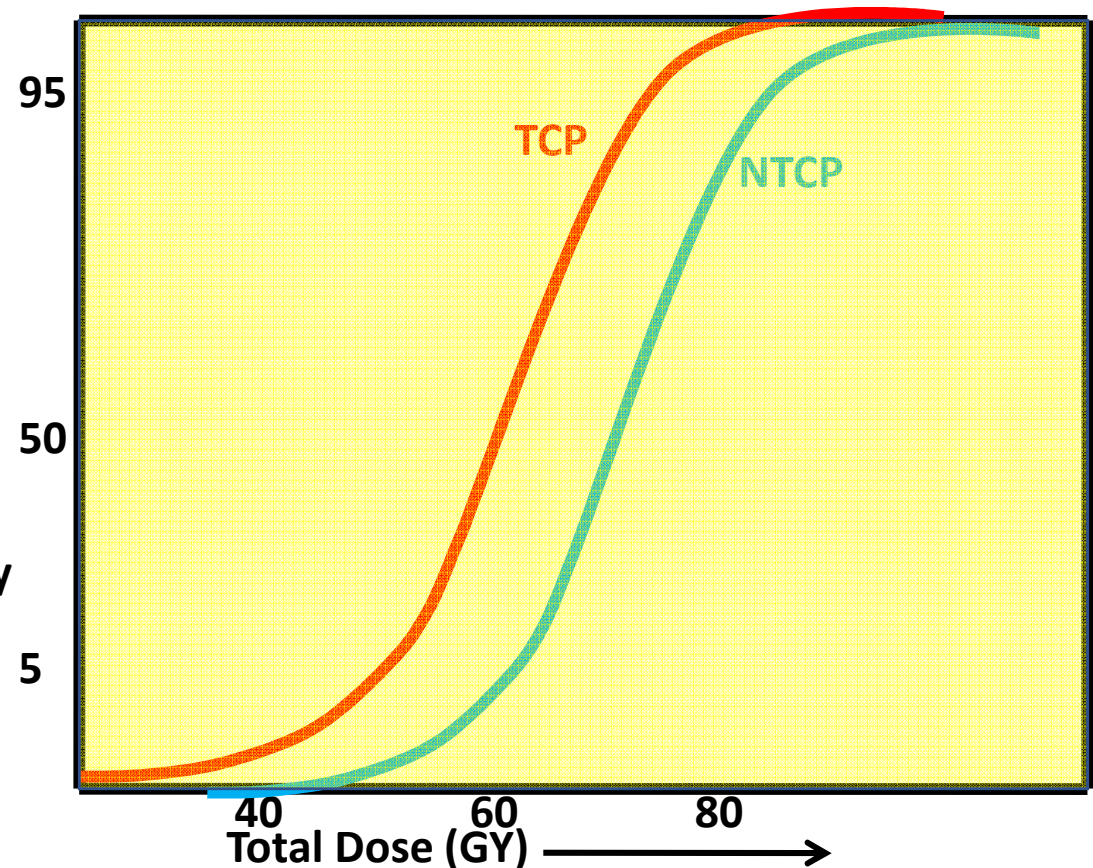
$$TR = \frac{(TCP)}{(NTCP)}$$

Dose Response Curve is between probability of effect on one axis vs total dose of radiation on other axis

Dose Response curve is plotted for tumor and normal tissues are usually sigmoid or S shaped.

•Therapeutic Ratio may be

- Favorable***
- unfavorable***

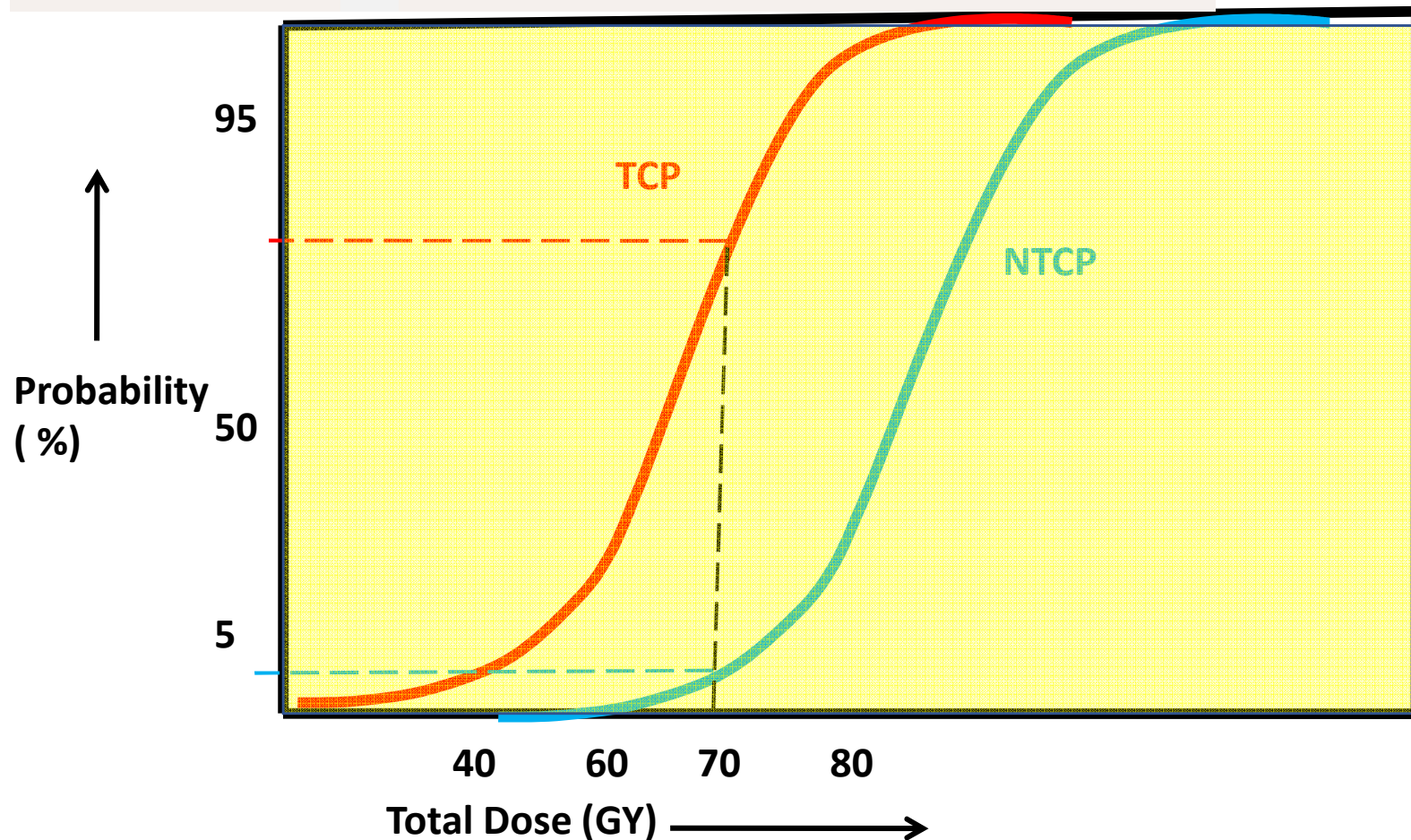


Favorable Therapeutic Ratio

➤ *TCP curve should be left and NTCP should be right*

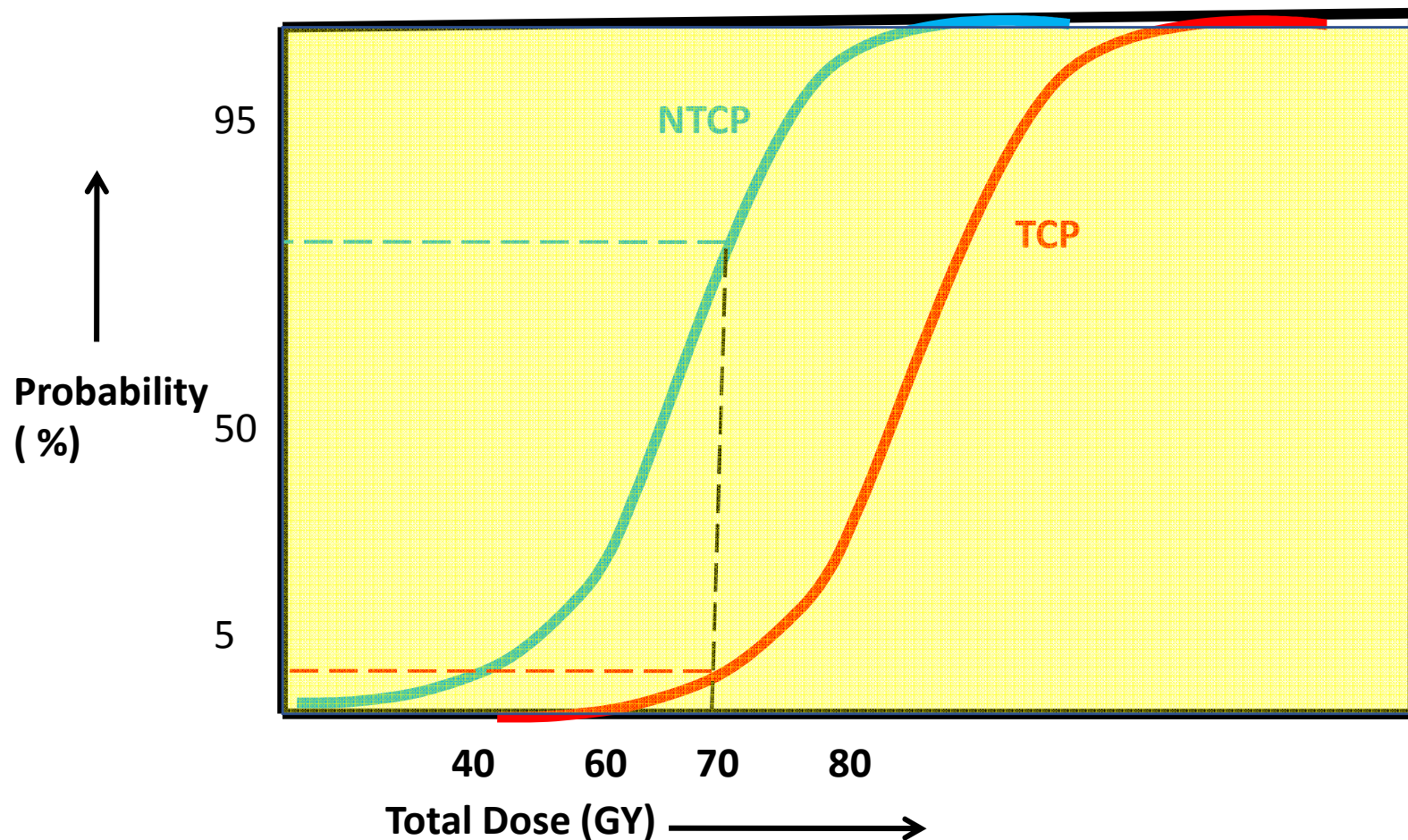
□ For a typical good radiotherapy treatment:

- $TCP \geq 0.5$ (50%)
- $NTCP \leq 0.05$ (5%)



Unfavorable Therapeutic Ratio

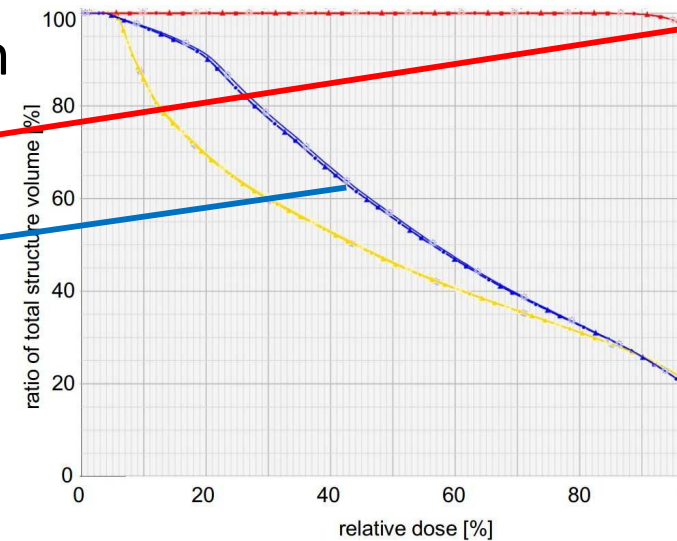
➤ *If for any clinical situation NTCP curve is on left and TCP is on right*



Introduction

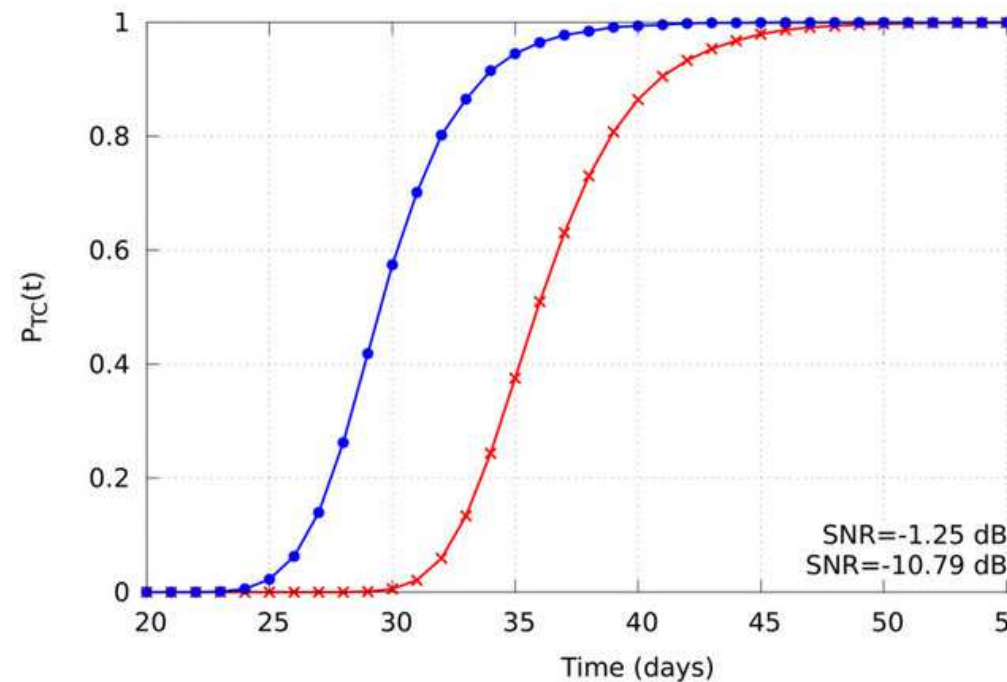
Dose Volume Histogram(DVH) reflect dose to volume of organ

Tumour
Normal Organ



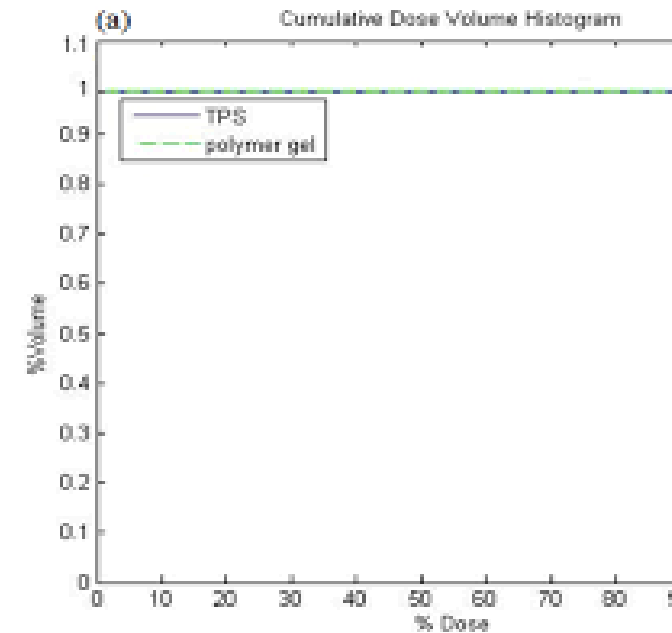
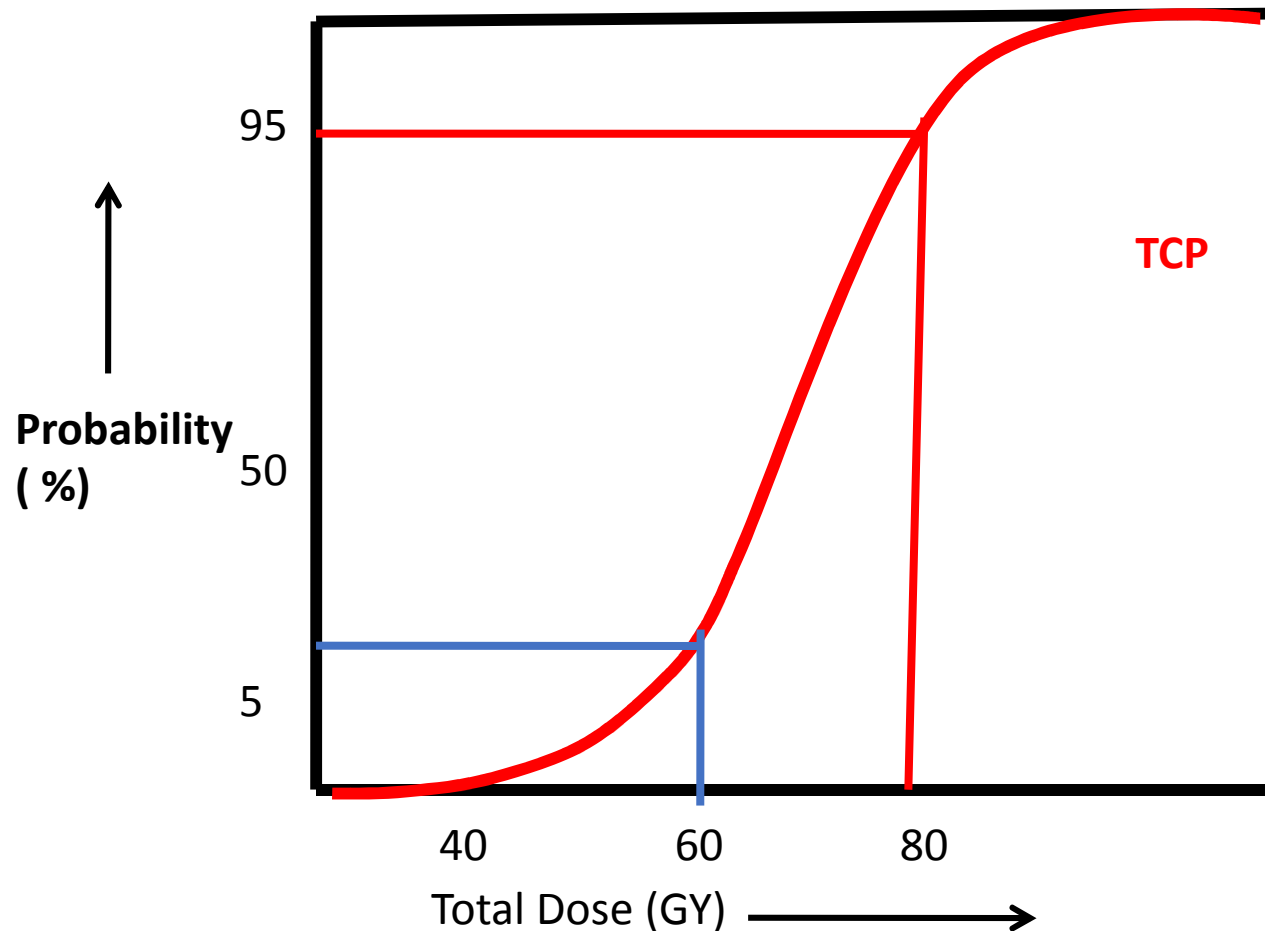
Tumour Control Probability (TCP)

Normal Tissue Complication Probability (NTCP)



Tumor Control Probability (TCP)

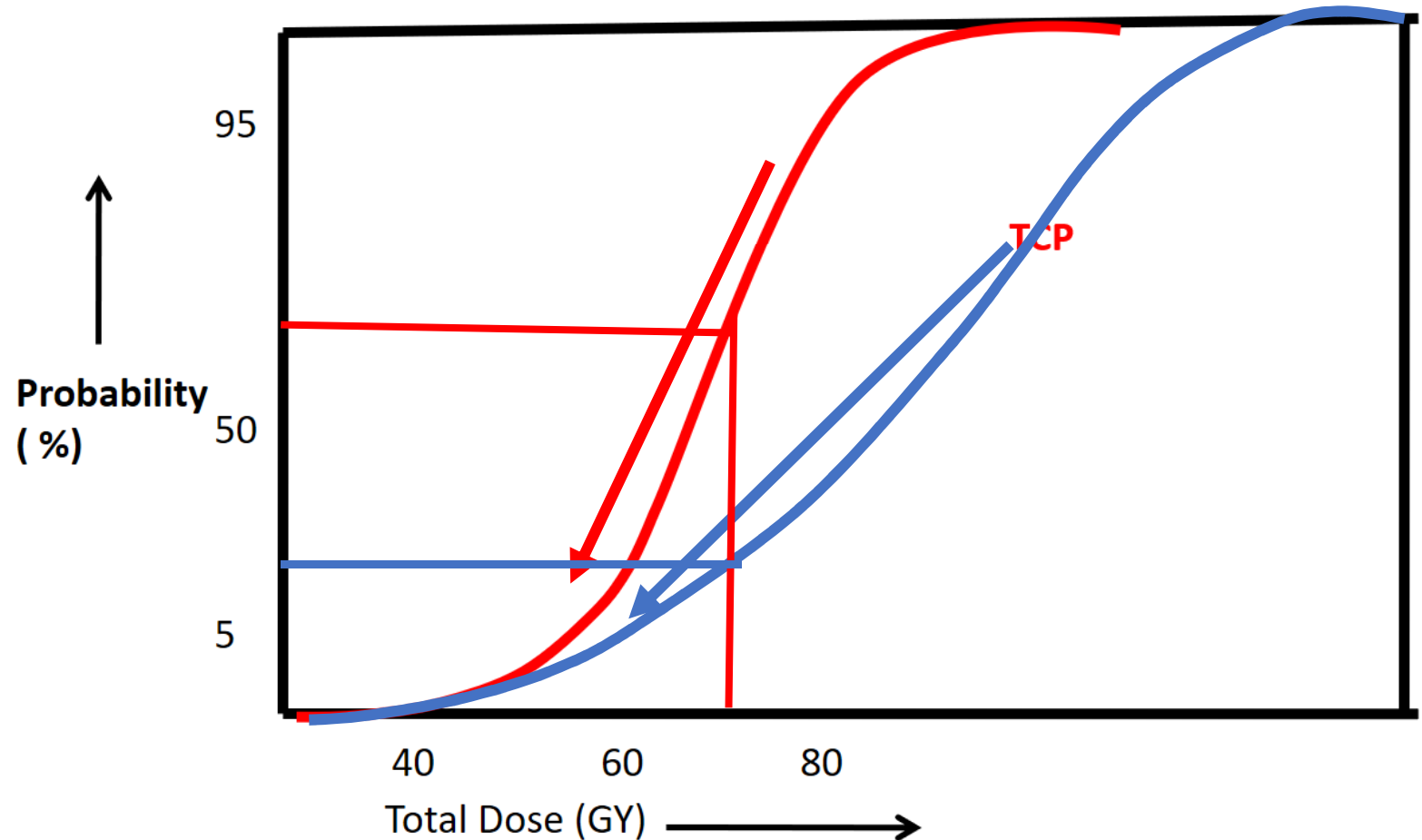
100% prescribed dose should cover 100 volume of Tumour



Sigmoid Curve for TCP

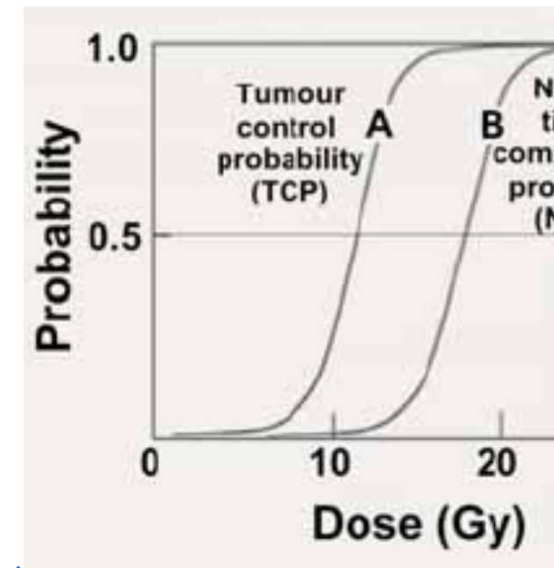
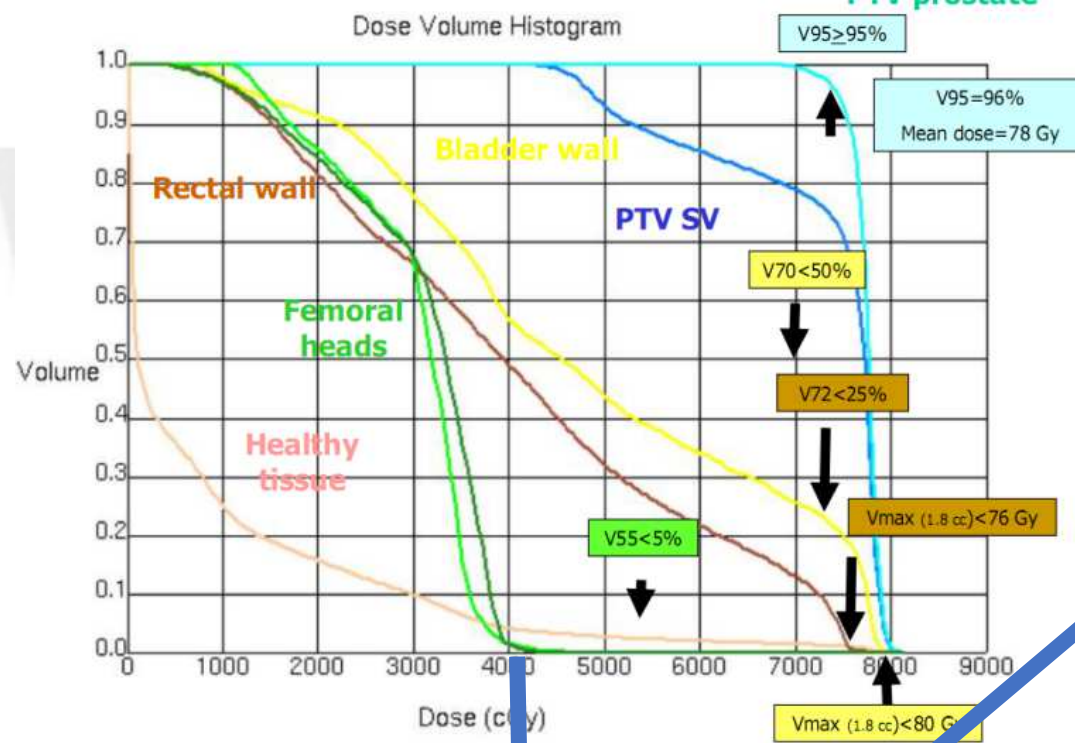
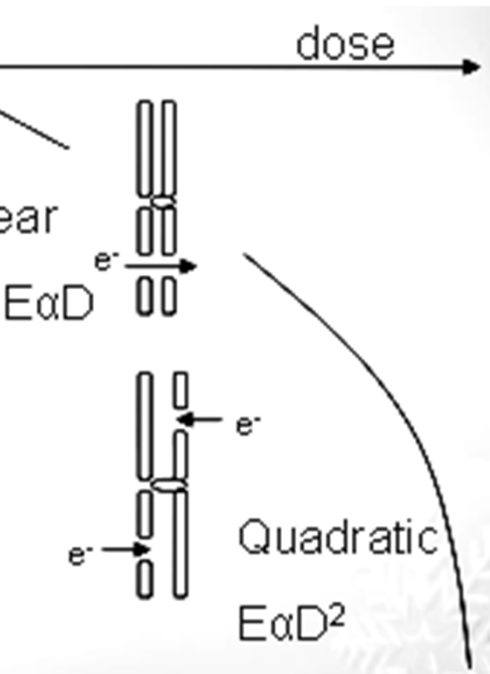
steepness of slope in clinical situation based on
clinical data is less than obtained experimentally

WHY ?



- This was attributed to the difference in radio sensitivity of the clonogenic cells in different patients k/as inter-patients heterogeneity.
- This is mainly due to variation in α values, which represent the intrinsic radiation sensitivity of an individual.
- Variation in number of clonogenic cells
- Variation in hypoxic fraction
- Variation in cell density
- etc.

r-quadratic model



Biological Model

radiobiological Models

- 1. There are number of radiobiological models developed for estimating normal tissue complication probability and tumor control probability but outcome of each model is not same.**
- 2. Most of RB models are based on following presumptions.**
 - a) Cell survival after irradiation is bionomial and obeys Poissons statistics.**
 - b) Response of an organ is determined by the death or survival of its target cells. (functional sub units for normal tissue and clonogens for tumors)**
 - c) All the target cells respond identically.**
 - d) If BED of two radiation schedule is same then end point will be independent of dose per fraction.**

Radiobiological Models

1. TCP models:

- a) The complication free tumor control objective, P_+
- b) Linear Quadratic Poissons cell kill model

2. NTCP models:

- a) Relative seriality model (s model)
- b) The k model
- c) The critical element model
- d) The critical volume model (Neimeirko)
- e) The Lyman, Kuthcer & Burman model (with fractionation & without fractionation effect)
- f) The parallel architecture model
- g) The Klepper & Klimanov mode

Linear Quadratic(L-Q) Model

$$F = e^{-(\alpha D + \beta D^2)}$$

$$F = N_s / N_o \quad N_s = \text{no of cell surviving} \quad N_o = \text{no of initial cells}$$

$$/ N_o = e^{-(\alpha D + \beta D^2)}$$

$$N_s = N_o e^{-(\alpha D + \beta D^2)}$$

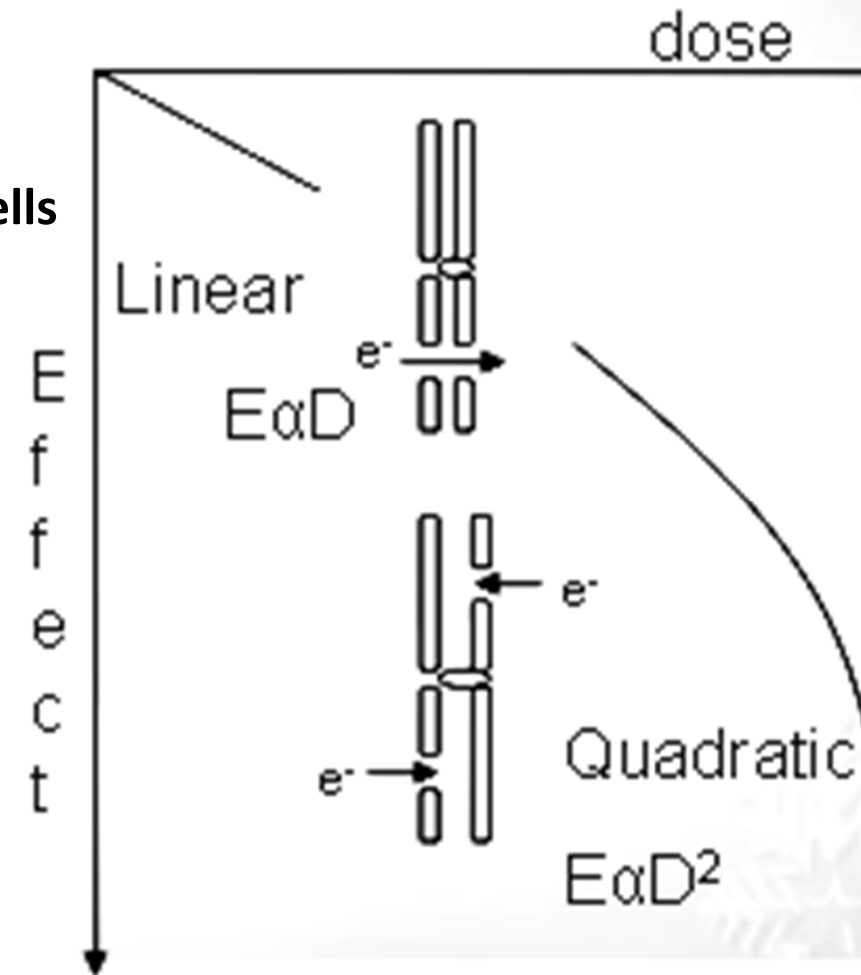
If n fx of dose d is given

$$N_s = N_o e^{-n(\alpha d + \beta d^2)}$$

$$N_s = N_o e^{-nd(\alpha + \beta d)}$$

$$N_s = N_o e^{-D(\alpha + \beta d)}$$

$$N_s = N_o \exp \left[-\alpha D \left(1 + \frac{\beta}{\alpha} d \right) \right]$$



Tumor Control Probability (TCP)

Poisson's Statistics $TCP = e^{-N_s}$ \longrightarrow Average number of surviving cells

$F = N_s / N_o$ N_s = no of cell surviving N_o = no of initial cells

$$N_s = SF \times N_o$$

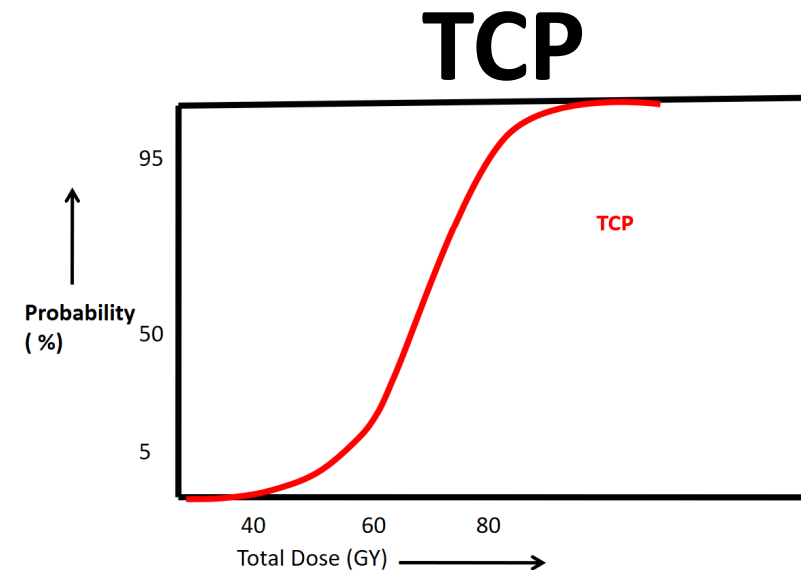
$$TCP = e^{-SF \times N_o}$$

$$F = e^{-(\alpha D + \beta D^2)}$$

$$TCP = \exp[-N_o \exp(-\alpha d - \beta d^2)] \quad \text{For single fraction of dose } d$$

For the case of n fractions, each of identical dose d such that $D_{tot} = d \times n$,

$$TCP = \exp \left\{ -N_o \exp \left[-\alpha D_{tot} \left(1 + \frac{\beta}{\alpha} d \right) \right] \right\}$$

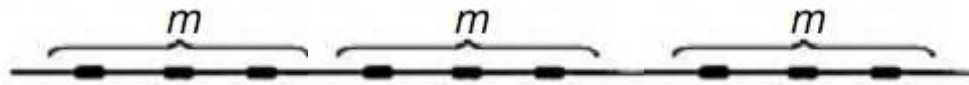


Parameters for TCP

- ❖ Value of α and β .
- ❖ Number of clonogenic cells
- ❖ Dose per fraction.
- ❖ Total dose.
- ❖ Standard deviation in α values.
- ❖ Inhomogeneous dose distribution.
- ❖ Inter fraction dose fluctuation due to set up uncertainties.
- ❖ Hypoxic component.
- ❖ Accelerated Repopulation
- ❖ Etc.

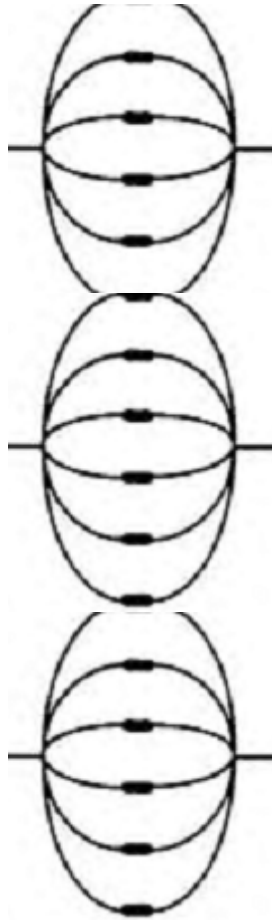
Normal Tissue Complication Probability (NTCP)

Functional Sub Unit (FSU) of Critical Organ



Serial like Spinal Cord

Volume of the organ is not important
and it is the dose which has got a
threshold, eg, spinal cord dose < 45 Gy.



Parallel like kidney

Volume of the organ is important
has got a threshold, eg, V20 of the
lung should be $< 30\%$.

Parallel FSU

- **Each FSU function independently.**
- **Clinical manifestation of radiation is evident only if small number of FSU survive.**
- **So there is always a threshold volume like V20 in lung etc. to be defined in radiation planning.**
- **Risk of complication depends upon the distribution of total dose in the organ and not on the hot spot at one place.**

Serial FSU

- **Function of the entire organ depends upon the function of each individual FSU.**
- **Inactivation of one FSU will result in clinical side effect.**
- **Risk of complication depends upon hot spot and not the dose distribution in entire organ.**
- **So Threshold dose is more important.**
- **Eg:- Spinal cord should get <45 Gy.**

LYMAN-KUTCHER-BURMAN (L-K-B) EMPIRICAL MODEL

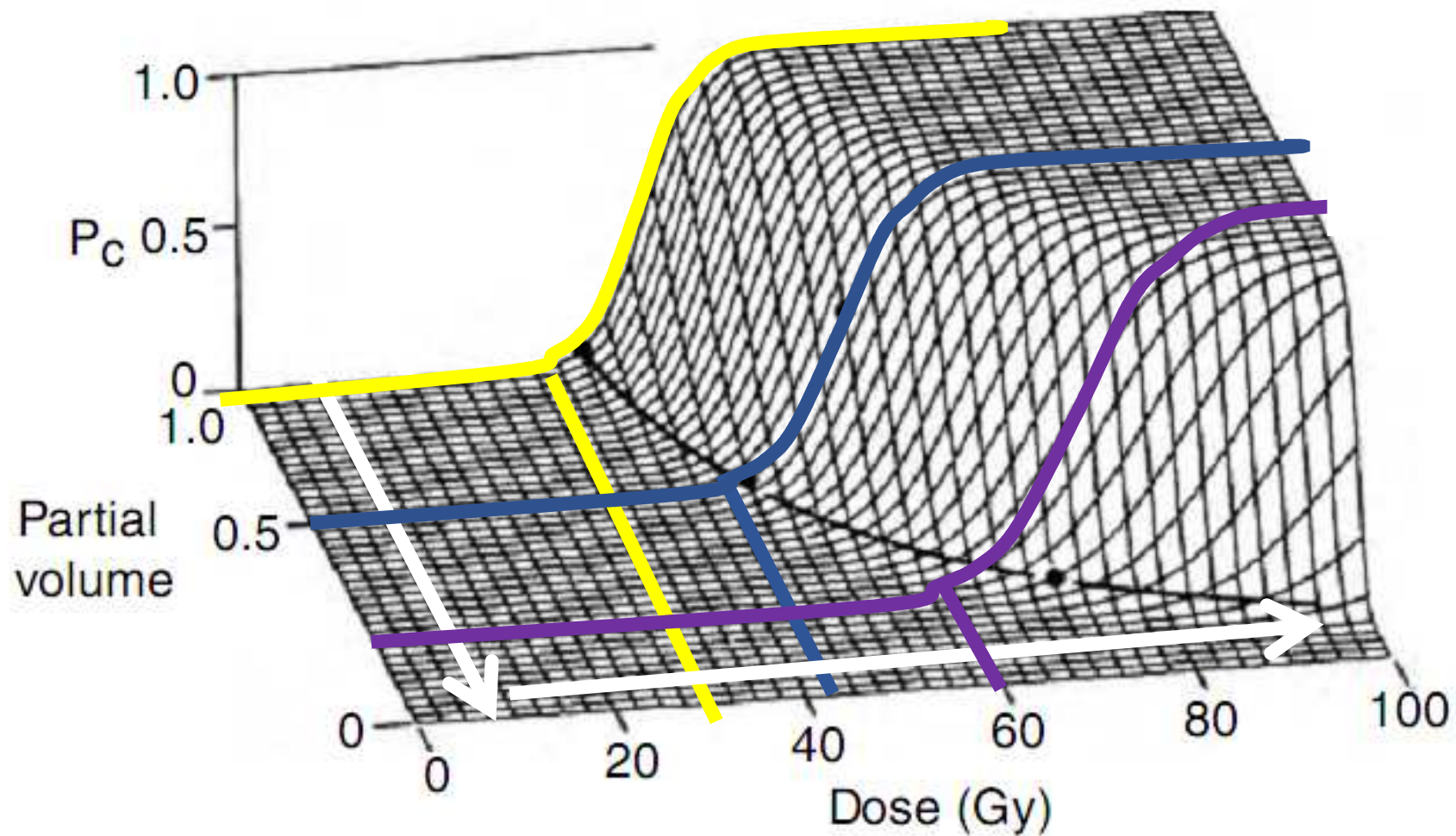
$$NTCP = \frac{1}{\sqrt{2\pi}} \int_{-\infty}^t e^{-t^2/2} dt$$

$$t = \frac{D - TD_{50}(V/V_{\text{ref}})}{m TD_{50}(V/V_{\text{ref}})}$$

$$TD_{50}(1) = TD_{50}(V/V_{\text{ref}})(V/V_{\text{ref}})^n$$

- $TD_{50}(1)$, the dose to the whole organ which would lead to complication in 50% of the population (note that $TD_{50}(V/V_{\text{ref}})$ is to be read as the TD_{50} at partial volume V/V_{ref});
- V_{ref} , a reference volume, which in many cases will be the (whole) organ volume;
- m , a parameter representing the steepness of the dose-response curve;

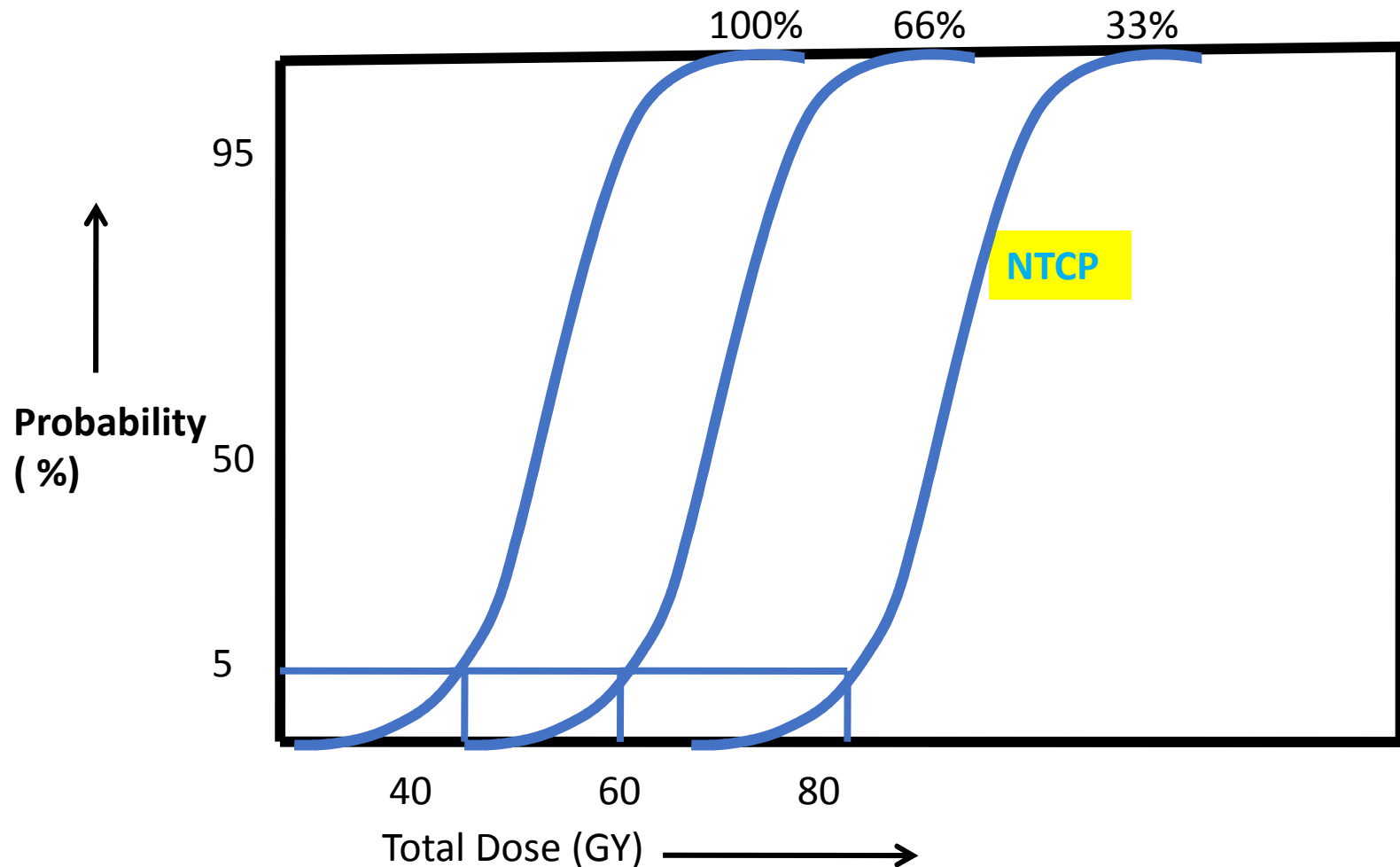
NTCP, Partial Volume and Dose Relationship for Heart



As partial volume decreases the sigmoid curve moves towards higher doses

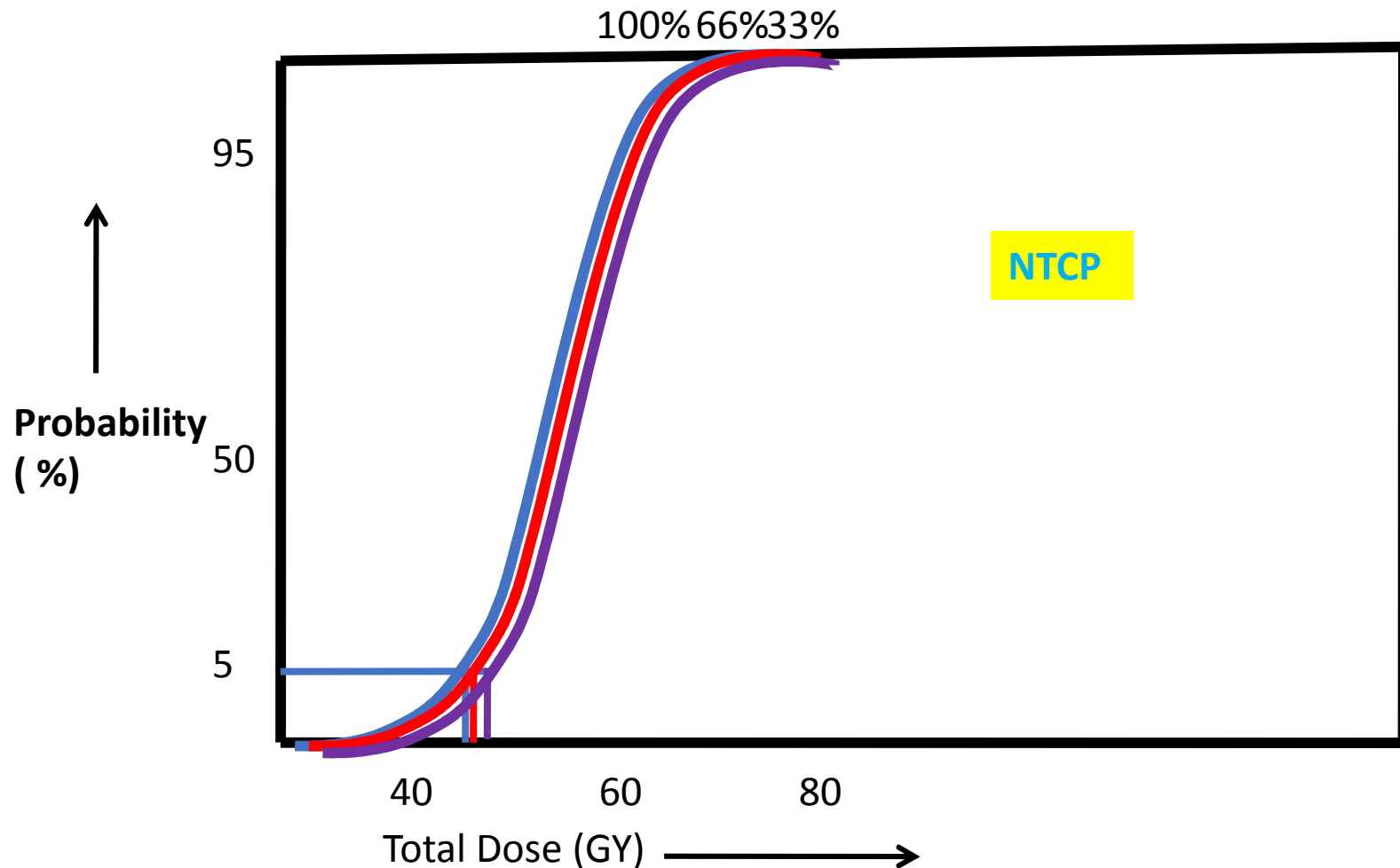
Volume effect for NTCP

This seen in parallel organ. Useful to have less no of fields so volume of the organ is kept low.



Volume effect for NTCP

This seen in Serial organs. Clinically useful to have many field so that dose distributed over larger volume but peak dose never reached.



What is RT Planning?

Basically radiotherapy planning has three stages.

- 1. First is fluence optimization**
- 2. Segmentation and dose calculation**
- 3. Plan evaluation**

Optimization.

1. Biological cost functions based.

Target

Poisson Cell Kill LQ Model

EUD (Equivalent Uniform Dose)

2. Physical Cost Function Based.

Max Dose

Min Dose

Mean Dose etc.

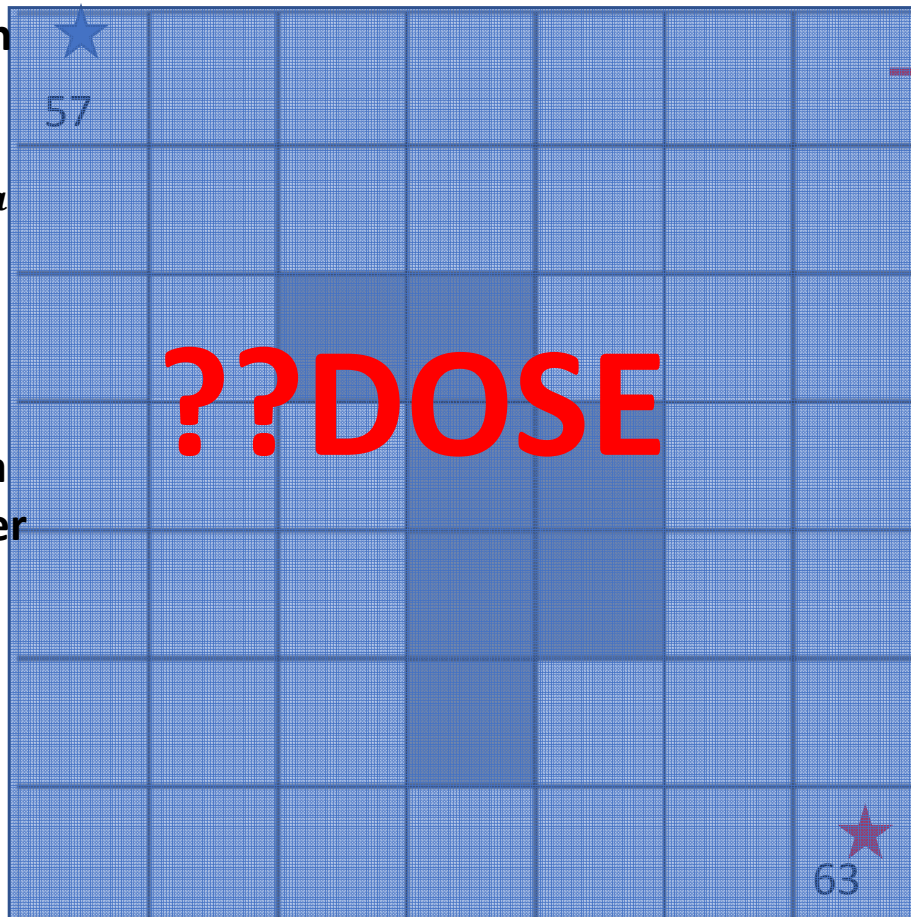
Equivalent Uniform Dose

EUD: the dose that, if distributed uniformly, will lead to the same biological effect as the actual non-uniform dose distribution.Niemierko, MP. 1997

Normalized EUD (gEUD) can be formulated as:

$$D = \left(\sum_i v_i D_i^a \right)^{1/a}$$

where v_i is the fractional organ volume receiving a dose D_i and a is a tissue-specific parameter that describes the volume



Voxel

Dose distribution +/- 5%

Dose = 60 Gy /30fx

70% control

Biological Cost functions

1. There are three Biological based treatment planning system (BBTPS) available till date.

1. Monaco

2. Pinnacle &

3. Eclipse.

Biological model used for treatment plan optimization in Monaco TPS (Elekta)

Structure Type	Name of model	Parameters	Comments
Target	Poissons statics cell kill model	Cell sensitivity (0.1-1.0 Gy ⁻¹) a Parameter i.e. tissue specific parameter	Mandatory biological component function for target no penalty for hot spots
AR	Serial complication model	Power law exponent (1-20)	Effective for controlling maximum organ dose (Point dose)
AR	Parallel complication model	Power law exponent (1-4)	Effective for controlling mean organ dose (Volume is important)

Biological model used for treatment plan optimization in PINNACLE (Philips)

Structure Type	Name of model	Parameters	Comments
Target	Min EUD	Volume parameter ($a < 1$)	Penalizes for too low EUD
Target	Target EUD	Volume parameter ($a < 1$)	Penalizes for a deviation from desired EUD
Organ at Risk	Max EUD	Volume parameter ($a \geq 1$)	Penalizes for too high EUD, use for both serial and parallel structures

Biological model used for treatment Plan Evaluation in PINNACLE (Philips)

Model name	Structure type	Name of model	Parameters/input
TCP/NTCP Monitor	Target OAR	Empirical TCP model Lyman-Kutcher model	D50, m D50, m, n
Biological response panel	Target OAR Multiple targets Multiple OARs Target & OARs	Poisson/LQ-based TCP model Kallman s-model Composite TCP Composite NTCP Probability of complication free tumor control	D50, γ , α/β

Biological model used for treatment plan optimization & plan evaluation in Eclipse (varian)

Structure Type	Name of model	Parameters	Comments
Target	Min EUD	Volume parameter (a)	Penalizes for too low value
Target or OAR	Max EUD	Volume parameter (a)	Penalizes for high value
Target	TCP Poisson-LQ	D50, γ , α/β , seriality(s), $T_{1/2}$ for short Vs long repair time, repopulation times: T_{pot} and T_{start}	To control TCP
OAR	NTCP Poisson-LQ	D50, γ , α/β , seriality (s), $T_{1/2}$ for short Vs long repair time, repopulation times: T_{pot} and T_{start}	To control NTCP
OAR	NTCP-Lyman	D50, m,n, α/β , $T_{1/2}$ for short Vs long repair time, repopulation times: T_{pot} and T_{start}	To control NTCP

Precaution while using RB models

- 1. Most NTCP models do not include dose per fraction effects. If the plan under evaluation is very different from that in dataset used to derive parameter estimates, both sets of data should be normalized to the same dose per fraction using LQ model formalism.**
- 1. If not corrected model can produce overestimates in NTCP if hyperfractionated and significantly underestimates if hypofractionated.**
- 1. Currently available TCP/NTCP models incorporated in BBTPS are not well documented and are not supplied with databases of reliable model parameters, so therefore have not generalized for clinical use.**



3rd ESTRO-AROI GYN Teaching Course

14th-17th March 2019

Department of Radiation Oncology

All India Institute of Medical Sciences, Rishikesh INDIA



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Thanks
Greetings From Rishikesh

